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Author(s)
Ueda, Masashi; Kudo, Takashi; Kuge, Yuji; Mukai, Takahiro; Tanaka, Shotaro; Konishi, Hiroaki; Miyano, Azusa; Ono, Masahiro; Kizaka-Kondoh, Shinae; Hiraoka, Masahiro; Saji, Hideo

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Rapid detection of hypoxia-inducible factor-1-active tumors: Pretargeted imaging with a protein degrading
in a mechanism similar to hypoxia-inducible factor-1α

Masashi Ueda¹, Takashi Kudo², Yuji Kuge²,³, Takahiro Mukai⁴, Shotaro Tanaka⁵, Hiroaki Konishi², Azusa
Miyano², Masahiro Ono², Shinae Kizaka-Kondoh⁵, Masahiro Hiraoka², Hideo Saji²

¹Radioisotopes Research Laboratory, Kyoto University Hospital, Faculty of Medicine, Kyoto University,
54 Shogoin Kawahara-cho, Kyoto 606-8507, Japan

²Department of Patho-Functional Bioanalysis, Kyoto University Graduate School of Pharmaceutical
Sciences, 46-29 Yoshida-Shimo-Adachi-cho, Sakyo-ku, Kyoto 606-8501, Japan

³Central Institute of Isotope Science, Hokkaido University, Kita 15, Nishi 7, Kita-ku, Sapporo 060-0815,
Japan

⁴Department of Biomolecular Recognition Chemistry, Graduate School of Pharmaceutical Sciences,
Kyushu University, 3-1-1 Maidashi, Higashi-ku, Fukuoka 812-8582, Japan

⁵Department of Radiation Oncology and Image-applied Therapy, Kyoto University Graduate School of
Medicine, 54 Kawahara-cho, Shogoin, Sakyo-ku, Kyoto 606-8507, Japan
Corresponding author:

Hideo Saji, PhD

Department of Patho-Functional Bioanalysis

Graduate School of Pharmaceutical Sciences

Kyoto University

46-29 Yoshida Shimoadachi-cho, Sakyo-ku, Kyoto 606-8501, Japan.

Phone: +81-75-753-4556, Fax: +81-75-753-4568

E-mail: hsaji@pharm.kyoto-u.ac.jp
Abstract

Purpose

Hypoxia-inducible factor-1 (HIF-1) plays an important role in malignant tumor progression. For the imaging of HIF-1-active tumors, we previously developed a protein—POS—which is effectively delivered to and selectively stabilized in HIF-1-active cells, and a radioiodinated biotin derivative—(3-\(^{123}\)I-iodobenzoyl)norbiotinamide (\(^{123}\)I-IBB)—which can bind to the streptavidin moiety of POS. In this study, we aimed to investigate the feasibility of the pretargeting method using POS and \(^{123}\)I-IBB for early imaging of HIF-1-active tumors.

Methods

Tumor-implanted mice were pretargeted with POS. After 24 h, \(^{125}\)I-IBB was administered and subsequently, the biodistribution of radioactivity was investigated at several time points. In vivo planar imaging, comparison between \(^{125}\)I-IBB accumulation and HIF-1 transcriptional activity, and autoradiography were performed at 6 h after the administration of \(^{125}\)I-IBB, which was administered 24 h after the administration of POS. The same sections that were used in autoradiographic analysis were subjected to HIF-1α immunohistochemistry.

Results

\(^{125}\)I-IBB accumulation was observed in tumors of mice pretargeted with POS (1.6% injected dose/g (%ID/g) at 6 h). This result is comparable to the data derived from \(^{125}\)I-IBB-conjugated POS-treated mice (1.4%ID/g at 24 h). In vivo planar imaging provided clear tumor images. The tumoral accumulation of
$^{125}\text{-IBB}$ significantly correlated with HIF-1-dependent luciferase bioluminescence ($R = 0.84$, $P < 0.01$).

The intratumoral distribution of $^{125}\text{-IBB}$ was heterogeneous and significantly correlated with HIF-1α-positive regions ($R = 0.58$, $P < 0.0001$).

**Conclusion**

POS pretargeting with $^{125}\text{-IBB}$ is a useful technique in the rapid imaging and detection of HIF-1-active regions in tumors.

**Key Words:**

Tumor hypoxia, Hypoxia-inducible Factor-1 (HIF-1), Oxygen-dependent degradation (ODD), Molecular imaging, Pretargeting
Introduction

Insufficient blood supply to a rapidly growing tumor leads to the presence of an oxygen tension below physiological levels, hypoxia in solid tumors [1]. Tumor hypoxia is critically important in tumor physiology and cancer treatment, and it appears to be strongly associated with malignant progression and therapy resistance. The transcription factor, hypoxia-inducible factor-1 (HIF-1) is induced in a hypoxic region; it is a master regulator of the genes that encode for angiogenic and metastatic factors, and plays an important role in tumor progression [2-4]. Thus, noninvasive imaging of HIF-1-active regions in tumors will be useful for characterizing tumors and determining a course of therapy.

HIF-1 is a heterodimer that consists of an oxygen-sensitive alpha subunit (HIF-1α) and a constitutively expressed beta subunit. In normoxia, two proline residues in the oxygen-dependent degradation domain (ODD) of HIF-1α are hydroxylated, leading to a proteasomal degradation of HIF-1α. Under hypoxic conditions, oxygen is the rate-limiting factor for prolyl hydroxylation, resulting in a decreased degradation of HIF-1α [5, 6]. That is to say, the ODD of HIF-1α is responsible for the regulation of HIF-1 activity. Thus, it is likely that a probe containing ODD and degrading in a manner similar to HIF-1α does can be used to evaluate HIF-1 activity in vivo.

We have recently developed proteins in which the protein transduction domain (PTD) is fused to the ODD and demonstrated the specificity of these proteins to HIF-1-active cells [7-11]. In a previous study, we have also fused the PTD-ODD with a monomeric streptavidin (SAV), to produce a chimeric protein, PTD-ODD-SAV (POS); we also synthesized a radiolabeled biotin derivative,
(3-123/125I-iodobenzoyl)norbiotinamide (123/125I-IBB). For nuclear medical imaging, the two were conjugated (123/125I-IPOS); the characterization thereof has been presented previously [9]. In brief, POS was degraded in an oxygen-dependent manner and a clear tumor image was obtained 24 h post-injection of 123I-IPOS; additionally, the tumoral accumulation correlated with HIF-1 activity and the intratumoral distribution of 125I-IPOS was heterogeneous and corresponded to hypoxic areas. These findings suggested that 123I-IPOS is a potential probe for the imaging of HIF-1-active tumors. However, due to its large molecular size, 123I-IPOS cleared from the blood slowly; thus, we could not obtain a high tumor-to-normal tissue ratio within a short time after probe injection.

To overcome this problem, we propose a pretargeting method based on the high-affinity interaction between streptavidin and biotin [12]. This method uses a combination of tumor-seeking molecules and the prompt clearance of low-molecular-weight radiolabeled compounds (effector molecules) that are cleared within minutes from the blood. One of the advantages of the pretargeting method is that this method provides a high tumour-to-normal tissue ratio within a short time after injection. In addition, because the effector molecules used in this method are rapidly cleared from the body, the radiation exposure reduces. Moreover, some recent studies have shown that the tumor uptake of the effector molecules used in the pretargeting method was achieved identical to or even higher than that of directly radiolabeled antibody. The images and therapeutic effects reported by these studies were significantly improved [13-15]. In the present study, we aimed to reveal the effectiveness of the pretargeting method using POS and 123I-IBB, in the rapid imaging of HIF-1-active tumor hypoxia.
Materials and Methods

Cell and cell culture

FM3A mouse mammary tumor cells were purchased from Health Science Research Resources Bank (Osaka, Japan) and were cultured in 10% fetal bovine serum (FBS)-RPMI 1640 medium (Nissui Pharmaceutical, Tokyo, Japan). Suit2 human pancreatic tumor cells that express luciferase in response to HIF-1 activity (Suit2/Luc cells) were established by Prof. Kizaka-Kondoh [16]. These cells were authenticated by multi plex PCR method using short tandem repeat and were maintained in 10% FBS-Dulbecco’s modified Eagle’s medium (Nissui Pharmaceutical). The culture media were supplemented with penicillin (100 units/mL) and streptomycin (100 μg/mL). Cells were incubated at 37°C in a well-humidified incubator with 5% CO₂ and 95% air.

Preparation of fusion protein

POS was overexpressed in Escherichia coli and purified as described in a previous report [9]. Purified POS was then dissolved in Tris-HCl buffer (pH 8.0).

Synthesis

Ammonium ^{123}I-iodide was kindly provided by Nihon Medi-Physics (Hyogo, Japan). Sodium
125I-iodide was purchased from PerkinElmer Life and Analytical Sciences (Boston, MA). All other chemicals used in this study were of reagent grade and are commercially available. 123/125I-IBB and non-radioactive IBB were synthesized as described in a previous report [9, 17]. 123I-IPOS was obtained by incubating 123I-IBB and POS for 1 h, followed by purification with Sephadex G50 columns (GE Healthcare Bioscience, Uppsala, Sweden).

Animal model

Animal studies were conducted in accordance with our institutional guidelines, and the experimental procedures were approved by the Kyoto University Animal Care Committee. Five-week-old female C3H/He mice and BALB/c nu/nu mice were purchased from Japan SLC, Inc. (Hamamatsu, Japan). FM3A and Suit2/Luc tumor models were prepared as described in a previous report [9]. The cells were subcutaneously implanted in the right thighs, except in the case of the mice that were used for the bioluminescence imaging wherein the cells were subcutaneously implanted in both the thighs. After tumor implantation, mice were fed an AIN76-A-based, biotin-free diet (Oriental Yeast Co. Ltd., Tokyo, Japan) in order to prevent dietary biotin from inhibiting the binding of 125I-IBB to POS. The mice were subjected to a tracer study two weeks after implantation. The average diameter and average volume of the tumors were 8 mm and 350 mm³, respectively.

Biodistribution
I\textsuperscript{\textsubscript{25}}-IBB (37 kBq) was injected intravenously into FM3A-implanted mice ($n = 3$–$5$); at 1, 3, 6, and 24 h post-injection, the mice were sacrificed. For the pretargeting study, the mice ($n = 5$) were injected with 30 $\mu$g of POS and 24 h later, I\textsuperscript{\textsubscript{25}}-IBB was injected intravenously. The mice were sacrificed at the same time points as described above. Whole organ specimens were immediately removed and weighed, and their radioactivity was measured with an auto well gamma counter (ARC2000; Aloka, Co., Ltd., Tokyo, Japan). The results are expressed in terms of the percent injected dose per gram of tissue (%ID/g).

\textit{In vivo blocking study}

FM3A-implanted mice ($n = 5$) were pretargeted with POS (30 $\mu$g); 24 h later, I\textsuperscript{\textsubscript{25}}-IBB (37 kBq) was injected intravenously, with or without D-biotin (1 nmol) or with unlabeled IBB (500 pmol). Six hours after I\textsuperscript{\textsubscript{25}}-IBB administration, the mice were sacrificed. Whole organ specimens were immediately removed and weighed, and their radioactivity was measured with the gamma counter (ARC2000). The results are expressed as %ID/g.

\textit{Size-exclusion analysis of radioactive compounds in tumors}

FM3A-implanted mice ($n = 5$) were pretargeted with POS (30 $\mu$g); 24 h later, I\textsuperscript{\textsubscript{25}}-IBB (8.0 MBq) was injected intravenously. The mice were sacrificed 6 h after the injection of I\textsuperscript{\textsubscript{25}}-IBB, and the tumors were then removed. Extracts were prepared according to a previously reported method [18], with a slight modification. In brief, the tumors were homogenized in ice-cold 0.1 M Tris-HCl buffer containing 0.15 M
NaCl (pH 6.5), using a Polytron homogenizer (PT10-35, Kinematica AG, Switzerland); the preparations were then centrifuged at 4°C and 5,000 × g for 30 min (Micro Cooling Centrifuge 5922; Kubota, Osaka, Japan). The supernatants were filtered through a 0.46-μm filter (Nacalai Tesque, Kyoto, Japan) and analyzed by size-exclusion chromatography using a PD-10 column (GE Healthcare Bioscience).

**In vivo imaging**

SPECT-2000H scanner (Hitachi Medical Co., Tokyo, Japan) employing a low-energy, high-resolution, parallel-hole collimator [19, 20] was used. For direct targeting (n = 4), $^{123}$I-IPOS (30 μg, 4.9–7.4 MBq) was injected intravenously into each FM3A-implanted mouse. For the pretargeting method (n = 5), $^{123}$I-IBB (3.1–16 MBq) was injected into a tail vein 24 h after pretargeting with POS (30 μg). Under 2.5% of halothane anesthesia, the mice were placed on a scanner bed in the prone position. Planar images were obtained at 24 h after the injection of $^{123}$I-IPOS in mice belonging to the direct-targeted group or at 6 h after the injection of $^{123}$I-IBB in mice belonging to the pretargeted group. The image-acquisition time was 10 min for both the groups. Regions of interest (ROI) were set on the tumor in the right thigh and the corresponding area in the left thigh.

**Comparison between $^{125}$I-IBB accumulationin and HIF-1 transcriptional activity within identical tumors in mice pretargeted with POS**

The Suit2/Luc-implanted mice (n = 5) were pretargeted with POS (30 μg) and 24 h later, $^{125}$I-IBB
(37 kBq) was injected intravenously. After 5.5 h, 200 μL of d-luciferin solution (10 mg/mL in PBS; VivoGlo Luciferin, Promega, Wisconsin) was injected intraperitoneally. After 20 min, the mice were anesthetized with 2.5% isoflurane and imaged according to a previously described method [9]. After bioluminescence imaging, the mice were sacrificed and the radioactivity in each tumor was measured.

**Autoradiography**

Autoradiographic studies were performed in Suit2/Luc-implanted mice (n = 6). The mice were pretargeted with POS (30 μg) and 24 h later, $^{125}$I-IBB (4.1 MBq) was injected intravenously. After another 4 h, pimonidazole (PIMO, 60 mg/kg) was injected intraperitoneally and the mice were sacrificed 2 h later. Autoradiograms were then obtained and analyzed, according to a previously described method [19-21]. The adjacent section on each autoradiogram was stained with hematoxylin–eosin to identify regions of necrosis.

**Immunohistochemistry**

The slides used in the autoradiographic study were subjected to dual fluorescent immunostaining for HIF-1α and PIMO. The sections were fixed in 2% paraformaldehyde and ice-cold methanol, blocked with Protein Block Serum Free (Dako, Glostrup, Denmark), and treated with anti-human/mouse HIF-1α polyclonal antibody (R&D Systems, Minneapolis, MN) as a primary antibody; the specific signals were detected using an Alexa Fluor 568-conjugated F(ab′)$_2$ fragment of goat anti-rabbit antibody (Invitrogen,
San Diego, CA). Thereafter, after washing with PBS, FITC-conjugated mouse IgG1 monoclonal antibody (Chemicon, Temecula, CA) was treated according to the manufacturer’s protocol for PIMO staining. The sections were then dried and coverslipped using an antifade reagent (ProLong Gold; Invitrogen). To evaluate the specificity of the HIF-1α signal, negative control rabbit immunoglobulin (Dako) was incubated with the adjacent sections, instead of the primary antibody. To evaluate the specificity of the PIMO signal, tumor sections derived from PIMO-untreated mice were stained by following the same protocol. Fluorescent microscopic images were obtained by BIOREVO BZ-9000 (Keyence Corp., Osaka, Japan).

Image analysis

The autoradiograms were quantified using MultiGauge software (ver. 3.0, Fuji Photo Film Co., Ltd., Tokyo, Japan) and the immunohistochemical images were analyzed using BZ analyzer software (Keyence Corp.). ROIs were set on identical positions in both images on the basis of the x- and y-position of each ROI displayed in the both softwares. The necrotic regions were excluded from the analysis. We set 10–14 ROIs (area, 1-mm²) on the autoradiogram of each tumor and then transferred them to the corresponding immunohistochemical image. The radioactivity in each ROI was expressed in terms of %ID. The expression densities of HIF-1α and PIMO were determined in terms of the percentage of the positively stained region.
Statistical analyses

Comparisons between the two groups were made using the Mann-Whitney \( U \) test, and correlation coefficients were assessed using the Spearman rank analysis. A Chi-square test was used to compare the correlation coefficients between \(^{125}\text{I}-\text{IBB} \) accumulation and HIF-1\( \alpha \) expression or PIMO adduct-formation. \( P < 0.05 \) was considered statistically significant.

Results

Radiosynthesis of \(^{123}\text{I} - \text{IBB} \) and \(^{123}\text{I}-\text{IPOS} \)

\(^{123}\text{I}-\text{IBB} \) and \(^{125}\text{I}-\text{IBB} \) were obtained in the absence of a carrier and with radiochemical yields of 29\% and 65\% and radiochemical purities of greater than 95\% and greater than 94\%, respectively. \(^{123}\text{I}-\text{IPOS} \) was obtained with a radiochemical yield of 90\% and a radiochemical purity of greater than 99\%.

Biodistribution

An examination of the biodistribution of \(^{125}\text{I}-\text{IBB} \) alone revealed that the tumor-to-blood ratio was less than 1 at all time points. This indicated that \(^{125}\text{I}-\text{IBB} \) did not accumulate in the tumors. The radioactivity in the stomach was low; this indicates the resistance of \(^{125}\text{I}-\text{IBB} \) to deiodination \textit{in vivo} (Table 1). In contrast, in the pretargeted group, the tumor-to-blood ratio was greater than 1 as early as 1 h after the injection of \(^{125}\text{I}-\text{IBB} \) and the tumor-to-blood ratio had increased in a time-dependent manner (Table 2). The
blood clearance in both groups was comparable. In the pretargeted group, tumor accumulation of $^{125}$I-IBB at 6 h post-injection was $1.58 \pm 0.42\%$ID/g, which was more than 30-fold higher than the case of $^{125}$I-IBB alone ($0.05 \pm 0.01\%$ID/g). The radioactivity in the normal tissues decreased more rapidly than that in the tumor. The radioactivity in the tumor at 24 h after injection was the second highest among organs examined and both the tumor-to-blood and tumor-to-muscle ratios further increased (Table 2).

The tumoral uptake of $^{125}$I-IBB was significantly reduced to 46%, through the treatment with non-radioactive IBB (Table 3). A concomitant treatment with d-biotin also resulted in a 37% decrease in the tumoral uptake of $^{125}$I-IBB (Data not shown). The $^{125}$I-IBB accumulation in other tissues, except in blood, decreased on the treatment with non-radioactive IBB.

**Size-exclusion analysis of radioactive compounds in tumors**

The recovery of radioactivity from tumor homogenates was $95.7 \pm 7.2\%$, and that from the PD-10 columns was $85.5 \pm 6.9\%$. A major proportion of the radioactivity was eluted in a macromolecular fraction ($78.7 \pm 6.7\%$).

**In vivo imaging**

Fig. 1A illustrates the accumulation of $^{123}$I-IBB in the POS-pretargeted tumor. The tumor was clearly visualized 6 h after $^{123}$I-IBB injection, and the calculated tumor-to-muscle ratio was $4.6 \pm 1.4$. The image was comparable to that obtained 24 h after $^{123}$I-IPOS injection, using the direct-targeting method.
(Fig. 1B; tumor-to-muscle ratio, 6.9 ± 1.6). Compared to the direct targeting method, with the pretargeting method, radioactivity in the liver decreased, but increased in the intestine. These findings were consistent with the biodistribution study data.

$^{125}$I-IBB accumulation vs. HIF-1 transcriptional activity in tumors in mice pretargeted with POS

Figure 2 shows a positive correlation between HIF-1-induced luciferase bioluminescence and $^{125}$I-IBB accumulation at 6 h post-injection in tumors in mice pretargeted with POS ($R = 0.84$, $P < 0.01$).

Regional distribution of $^{125}$I-IBB in the POS-pretargeted tumor

Dual fluorescent immunohistochemistry revealed the presence of HIF-1$\alpha$- and PIMO-positive hypoxic areas in the tumor (Fig. 3A, B). The sections derived from PIMO-untreated mice were not stained with anti-PIMO antibody, and the HIF-1$\alpha$ signal was not detected in the negative control antibody-treated sections (data not shown). The autoradiogram showed that the distribution of $^{125}$I-IBB in the tumor was heterogeneous (Fig. 3C) and, for the most part, corresponded to the HIF-1$\alpha$- or PIMO-positive hypoxic areas. However, there were also a few regions where the signal of HIF-1$\alpha$ or PIMO was positive, but where $^{125}$I-IBB had not accumulated (Fig. 3D, E). High-magnification merged imaging of HIF-1$\alpha$ and PIMO immunostaining revealed that HIF-1$\alpha$-positive regions and PIMO-positive regions were not always identical; some regions were positive for both, while other regions did not match (Fig. 3F). Therefore, we compared correlations between $^{125}$I-IBB accumulation and expressions of HIF-1$\alpha$ or PIMO. As shown in
Fig. 4, significantly positive correlations were found between the regional accumulation of $^{125}$I-IBB in POS-pretargeted tumor sections and the expression of both hypoxic markers (HIF-1α: $R = 0.58$, $P < 0.0001$; PIMO: $R = 0.34$, $P < 0.005$). The correlation coefficient between $^{125}$I-IBB and HIF-1α was greater than that with PIMO, though the difference was not statistically significant ($\chi^2 = 3.13$, $P = 0.077$).

**Discussion**

Here we show early-phase tumor imaging afforded by pretargeting using POS and $^{123/125}$I-IBB. Using the pretargeting method, the tumoral accumulation (1.6%ID/g) and the tumor-to-blood ratio (4.2) at 6 h post-injection were found to be comparable to the data obtained 24 h after $^{125}$I-IPOS injection (1.4%ID/g, 5.1) [9]. The scintigraphic images of mice targeted with $^{123}$I-IPOS were very similar to those of prior studies, in which high signal levels were detected in the tumor—although the highest activity accumulated in the liver, even 24 h post-injection [9]. In contrast, the images of the pretargeted mice clearly demonstrate that $^{123}$I-IBB accumulated in the tumor more rapidly and cleared much more promptly from the body—with the exception of the intestine—than did the $^{123}$I-IPOS. These results indicate that the pretargeting method allows a shortening of the waiting time to one-fourth that required by direct targeting, in obtaining an adequate image. Clinical application of the pretargeting method in the future will contribute to reduction in radiation exposure of a patient.

Recently, it has been suggested that HIF-1 activates a number of genes—such as VEGF,
erythropoietin, matrix metalloproteinase, and glucose transporter—and that the expression level of HIF-1 correlates with poor prognosis in many tumors [22-26]. Furthermore, the activation of such genes has an important role with respect to aggressive cancer phenotypes. Therefore, visualization and tumor therapy targeting for HIF-1 activation may be an important supplement to imaging of hypoxia per se, when characterizing tumors. Thus far, some hypoxia imaging probes—such as $^{18}$F-fluoromisonidazole ($^{18}$F-FMISO), 1-α-D-(5-deoxy-5-$^{18}$F-fluoroarabinofuranosyl)-2-nitroimidazole ($^{18}$F-FAZA), and $^{64}$Cu-diacetyl-bis(4-methylthiosemicarbazone) ($^{64}$Cu-ATSM)—have been developed [27]. They detect physically low oxygen pressure (<10 mmHg) and are useful in predicting efficacy of radiotherapy [28]. However, the mechanisms underlying hypoxic accumulation of such probes are not dependent on HIF-1 expression [29]. Previously reported HIF-1-activity imaging systems required exogenous reporter gene transcription, which presents difficulties in practice [30, 31]. In contrast, our approach could assess HIF-1-activity directly, via a two-step targeting of the probes.

A recent immunohistochemical study has demonstrated the lack of complete colocalization between HIF-1α and PIMO. Sobhanifar et al. report that HIF-1 expressed at higher levels of oxygen than those that allow PIMO metabolism and binding [32]. Thus, we compared the correlation between $^{125}$I-IBB accumulation and HIF-1α- or PIMO-positive regions. As shown in Fig. 4, the correlation coefficient between $^{125}$I-IBB and HIF-1α was greater than was the case with PIMO, although the difference between the 2 correlation coefficients was not statistically significant. Therefore, the $^{125}$I-IBB-accumulated regions potentially corresponded to the HIF-1α-positive regions but to a lesser degree with the PIMO-positive
regions. However, in the present study, the HIF-1α-positive region was mainly detected both in the PIMO-positive regions and in the regions surrounding them (Fig. 3F). The result is consistent with that of a previous study, which reports that carbonic anhydrase 9, a HIF-1-regulated protein, generally colocalized with PIMO though displaying greater extension in the direction of perfused areas [33]. Due to the overlap, the 125I-IBB-accumulated region also showed a weak positive correlation with the PIMO-positive regions. On the other hand, there were a few HIF-1α-negative regions in which 125I-IBB accumulated (Fig. 3D). This discrepancy could be explained by the delivery of POS and/or 125I-IBB. Since both probes were delivered by blood flow, they potentially tend to accumulate in blood-vessel-rich regions, i.e., HIF-1α-negative regions. Because the degradation rate of POS was relatively slow [9], an excess amount of POS delivered to HIF-1α-negative regions could not be degraded, resulting in 125I-IBB accumulation in those regions. POS contains not only the essential domain related to the oxygen-dependent degradation of HIF-1α, but also PTD and SAV. These modifications may lower the rate of degradation, and this is a drawback of POS. However, it should be noted that by using the pretargeting method with POS and 123I-IBB, the radioactivity accumulation significantly correlated with the HIF-1α-positive region (Fig. 4A). Furthermore, the accumulation of 123I-IBB correlated with HIF-1 transcriptional activity in the tumors in mice pretargeted with POS (Fig. 2). Thus, our approach would detect not only hypoxic regions, but also HIF-1-active regions; thus, this approach could prove important to the qualitative diagnosis of and effective therapy against cancer.

In the pretargeting study, 125I-IBB accumulated in the tumors of POS-pretargeted mice. The
accumulation was inhibited by non-radioactive IBB or \( \text{D}-\text{biotin} \). Moreover, most of the radioactivity in the tumor existed as macromolecules. Taken together, the radioactivity in the tumor is caused by the binding of \( ^{125}\text{I}-\text{IBB} \) to the SAV moiety of POS. Thus, \( ^{125}\text{I}-\text{IBB} \) has the ability to bind to streptavidin, not only \textit{in vitro} but also \textit{in vivo}. It was reported that the expression of HIF-1 is not ubiquitous, but heterogeneous, and is small in tumors [34]. The probe accumulation in the tumors harboring HIF-1-dependent reporter genes was approximately 1%ID/g in previous studies [34-36], which is comparable to the results of the present study.

In the biodistribution study of \( ^{125}\text{I}-\text{IBB} \) alone, the accumulation of radioactivity was highest in the intestine. This tissue distribution pattern reflects the behavior of radioiodinated biotin itself, since \( ^{125}\text{I}-\text{IBB} \) is not subjected to cleavage by serum biotinidase [17]. The high accumulation of \( ^{125}\text{I}-\text{IBB} \) in the intestine resulted in high background activity in the abdominal region; therefore, the imaging of abdominal HIF-1-active tumors would be difficult. In this case, biotin derivatives those show faster clearance from the abdominal region than \( ^{125}\text{I}-\text{IBB} \) is required. However, the background radioactivity in the thoracic region and cervicofacial region was considerably low. The expression of HIF-1 has been reported to be associated with a poor prognosis in breast and lung cancers and in head and neck squamous cell carcinomas [26, 37, 38]; therefore, our imaging approach would be particularly useful for detecting HIF-1 activity in those tumors.

Recent studies have revealed that HIF-1 level is controlled not only at the post-transcriptional level—that is, the oxygen-dependent regulation of the HIF-1\( \alpha \)—but also at the transcriptional and translational levels [39, 40]. In a region where the transcription and translation of HIF-1\( \alpha \) increased, an
excess amount of HIF-1α was likely to saturate the ubiquitin-proteasome degradation system and result in the upregulation of HIF-1, even in mild hypoxic conditions. This may be one reason why the threshold of oxygen pressure for HIF-1 stabilization is ambiguous and depends upon the character of the organs or tumors. In such regions, the POS degradation rate would also decrease, because it contains the ODD and degrades in the same manner as HIF-1α. Thus, in imaging with POS-pretargeting and 123I-IBB, it is possible to depict HIF-1-active regions that result from either hypoxic stabilization or the upregulation of transcription and translation.

Conclusion

Using the pretargeting method, clear tumor images were obtained in a shorter period of time than was possible with the direct-labeling method. Intratumoral accumulations of 125I-IBB in the POS-pretargeted tumors significantly correlated with HIF-1α-positive regions. These findings demonstrate that the pretargeting method with POS and 123I-IBB is effective for the rapid imaging of HIF-1-active tumor hypoxia.
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Conflict of interest

The authors have no conflict of interest.
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### Table 1. Biodistribution of $^{125}$I-IBB in FM3A-implanted mice

<table>
<thead>
<tr>
<th>Organ</th>
<th>Time after injection (h)</th>
<th>1</th>
<th>3</th>
<th>6</th>
<th>24</th>
</tr>
</thead>
<tbody>
<tr>
<td>Blood</td>
<td>1.12 ± 0.43</td>
<td>0.33 ± 0.01</td>
<td>0.15 ± 0.00</td>
<td>0.03 ± 0.01</td>
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</tr>
<tr>
<td>Liver</td>
<td>6.36 ± 1.70</td>
<td>1.21 ± 0.04</td>
<td>0.20 ± 0.04</td>
<td>0.02 ± 0.01</td>
<td></td>
</tr>
<tr>
<td>Heart</td>
<td>1.27 ± 0.31</td>
<td>0.26 ± 0.01</td>
<td>0.07 ± 0.04</td>
<td>0.02 ± 0.02</td>
<td></td>
</tr>
<tr>
<td>Lung</td>
<td>1.14 ± 0.22</td>
<td>0.30 ± 0.04</td>
<td>0.10 ± 0.03</td>
<td>0.02 ± 0.01</td>
<td></td>
</tr>
<tr>
<td>Kidney</td>
<td>5.54 ± 0.74</td>
<td>1.06 ± 0.23</td>
<td>0.35 ± 0.18</td>
<td>0.07 ± 0.02</td>
<td></td>
</tr>
<tr>
<td>Stomach</td>
<td>0.62 ± 0.13</td>
<td>0.35 ± 0.23</td>
<td>0.33 ± 0.24</td>
<td>0.12 ± 0.10</td>
<td></td>
</tr>
<tr>
<td>Intestine</td>
<td>32.61 ± 8.24</td>
<td>24.73 ± 12.12</td>
<td>10.69 ± 4.93</td>
<td>0.95 ± 0.64</td>
<td></td>
</tr>
<tr>
<td>Tumor</td>
<td>0.53 ± 0.14</td>
<td>0.13 ± 0.04</td>
<td>0.05 ± 0.01</td>
<td>0.01 ± 0.01</td>
<td></td>
</tr>
<tr>
<td>Muscle</td>
<td>0.84 ± 0.18</td>
<td>0.15 ± 0.05</td>
<td>0.03 ± 0.02</td>
<td>0.01 ± 0.01</td>
<td></td>
</tr>
<tr>
<td>Tumor/Blood</td>
<td>0.49 ± 0.14</td>
<td>0.39 ± 0.09</td>
<td>0.36 ± 0.09</td>
<td>0.57 ± 0.57</td>
<td></td>
</tr>
</tbody>
</table>

Organ uptake values are expressed as the percent injected dose per gram of tissue, except in the case of the stomach (the percent injected dose) and tumor/blood ratio. Values are represented as the mean ± S.D., $n = 3–5$. 
Table 2. Biodistribution of {superscript}125I-IBB in FM3A-implanted mice pretargeted with POS

<table>
<thead>
<tr>
<th>Organ</th>
<th>1</th>
<th>3</th>
<th>6</th>
<th>24</th>
</tr>
</thead>
<tbody>
<tr>
<td>Blood</td>
<td>1.28 ± 0.22</td>
<td>0.58 ± 0.05</td>
<td>0.37 ± 0.05</td>
<td>0.05 ± 0.01</td>
</tr>
<tr>
<td>Liver</td>
<td>10.16 ± 0.98</td>
<td>5.56 ± 0.74</td>
<td>4.07 ± 0.38</td>
<td>0.57 ± 0.15</td>
</tr>
<tr>
<td>Heart</td>
<td>1.77 ± 0.11</td>
<td>0.90 ± 0.12</td>
<td>0.59 ± 0.08</td>
<td>0.06 ± 0.02</td>
</tr>
<tr>
<td>Lung</td>
<td>1.98 ± 0.24</td>
<td>0.95 ± 0.13</td>
<td>0.67 ± 0.07</td>
<td>0.08 ± 0.01</td>
</tr>
<tr>
<td>Kidney</td>
<td>25.09 ± 1.42</td>
<td>11.58 ± 2.46</td>
<td>5.78 ± 1.02</td>
<td>0.30 ± 0.04</td>
</tr>
<tr>
<td>Stomach</td>
<td>0.63 ± 0.15</td>
<td>0.56 ± 0.17</td>
<td>0.34 ± 0.20</td>
<td>0.08 ± 0.05</td>
</tr>
<tr>
<td>Intestine</td>
<td>22.45 ± 3.40</td>
<td>20.11 ± 7.22</td>
<td>8.66 ± 6.13</td>
<td>0.76 ± 0.42</td>
</tr>
<tr>
<td>Tumor</td>
<td>2.73 ± 0.67</td>
<td>2.03 ± 0.16</td>
<td>1.58 ± 0.42</td>
<td>0.59 ± 0.23</td>
</tr>
<tr>
<td>Muscle</td>
<td>1.04 ± 0.16</td>
<td>0.47 ± 0.13</td>
<td>0.30 ± 0.11</td>
<td>0.04 ± 0.02</td>
</tr>
<tr>
<td>Tumor/Blood</td>
<td>2.15 ± 0.39</td>
<td>3.51 ± 0.26</td>
<td>4.23 ± 0.81</td>
<td>13.13 ± 4.58</td>
</tr>
</tbody>
</table>

Organ uptake values are expressed as the percent injected dose per gram of tissue, except in the case of the stomach (the percent injected dose) and tumor/blood ratio. Values are represented as the mean ± S.D., \( n = 5 \).
Table 3. Blocking study of the biodistribution of $^{125}$I-IBB in FM3A-implanted mice pretargeted with POS

<table>
<thead>
<tr>
<th>Organ</th>
<th>Vehicle</th>
<th>IBB treatment</th>
</tr>
</thead>
<tbody>
<tr>
<td>Blood</td>
<td>0.36 ± 0.18</td>
<td>0.48 ± 0.10</td>
</tr>
<tr>
<td>Liver</td>
<td>5.26 ± 0.61</td>
<td>2.58 ± 0.69*</td>
</tr>
<tr>
<td>Heart</td>
<td>0.76 ± 0.09</td>
<td>0.38 ± 0.08</td>
</tr>
<tr>
<td>Lung</td>
<td>1.09 ± 0.25</td>
<td>0.48 ± 0.12</td>
</tr>
<tr>
<td>Kidney</td>
<td>12.15 ± 5.03</td>
<td>2.44 ± 0.41**</td>
</tr>
<tr>
<td>Stomach</td>
<td>0.82 ± 0.48</td>
<td>0.25 ± 0.04</td>
</tr>
<tr>
<td>Intestine</td>
<td>9.04 ± 3.77</td>
<td>5.06 ± 2.30</td>
</tr>
<tr>
<td>Tumor</td>
<td>1.95 ± 0.63</td>
<td>0.90 ± 0.18*</td>
</tr>
<tr>
<td>Muscle</td>
<td>0.51 ± 0.06</td>
<td>0.16 ± 0.04†</td>
</tr>
<tr>
<td>Tumor/Blood</td>
<td>5.49 ± 1.12</td>
<td>1.93 ± 0.38‡</td>
</tr>
</tbody>
</table>

Organ uptake values are expressed as the percent injected dose per gram of tissue, except in the case of the stomach (the percent injected dose) and tumor/blood ratio. Values are represented as the mean ± S.D., n = 5.

*P < 0.005, **P < 0.001, †P < 0.0005, ‡P < 0.0001 vs. Vehicle group
Figures

Fig. 1

Typical planar images of FM3A-implanted mice, acquired through the pretargeting method (A) and the direct-targeting method (B). Images were acquired 6 h post-injection of $^{123}$I-IBB in the pretargeting method and 24 h post-injection of $^{123}$I-IPOS in the direct targeting method. Tumors were clearly visualized in a similar fashion in both images (arrow). Arrowheads indicate the intestine in A and the liver in B.
Correlation between $^{125}\text{I}-\text{IBB}$ accumulation and HIF-1 transcriptional activity within identical tumor in mice pretargeted with POS. Mice carrying tumors with the HIF-1-dependent luciferase reporter gene in both thighs were used. Ordinate represents accumulated radioactivity (%ID), and abscissa represents HIF-1-dependent luciferase bioluminescence. Correlation coefficient (R) was 0.84, indicating highly significant correlation ($P < 0.01$).
Fig. 3

Comparison between the intratumoral distribution of $^{125}$I-IBB and the HIF-1$\alpha$- or the pimonidazole (PIMO)-positive hypoxic regions, in POS-pretargeted tumors. The typical images of HIF-1$\alpha$ immunostaining (A), PIMO immunostaining (B), and autoradiogram (ARG; C) in the identical section are shown. Merged images of ARG with HIF-1$\alpha$ immunostaining or PIMO immunostaining are also shown (D and E, respectively). A high-magnification merged image of HIF-1$\alpha$ immunostaining with PIMO immunostaining (F, from insets in D and E) show that some regions were both positive (yellow) while others did not match (red or green).
Correlation between $^{125}$I-IBB accumulated area and HIF-1$\alpha$- or PIMO-positive area in POS-pretargeted tumors. A total of 6 sections (1 section per tumor) were analyzed. Quantitative analysis of autoradiograms provided data vis-à-vis $^{125}$I-IBB accumulation, expressed as %ID. A simple regression analysis of $^{125}$I-IBB accumulation with HIF-1$\alpha$ or PIMO expression showed a directly proportional relationship (HIF-1$\alpha$: $R = 0.58$, $P < 0.0001$; PIMO: $R = 0.34$, $P < 0.005$).