

1 **Association of alveolar nitric oxide levels with pulmonary function and its**  
2 **reversibility in stable asthma**

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14 Short title: **Association of alveolar NO with pulmonary function in asthma**

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22 **Key Words:** airway reversibility, alveolar NO, asthma, impulse oscillometry system,  
23 peripheral airway dysfunction, trumpet model with axial diffusion

24

25 **Abstract**

26 **Background:** Inflammation of peripheral airways is implicated in the pathophysiology  
27 of severe asthma. However, contributions of peripheral airway inflammation to airway  
28 caliber/function in patients with stable asthma, including those with mild to moderate  
29 disease, remain to be confirmed.

30 **Objectives:** To determine whether peripheral airway inflammation affects airway  
31 function in patients with asthma.

32 **Methods:** In 70 patients with mild to severe asthma, alveolar nitric oxide ( $C_{ANO(TMAD)}$ )  
33 levels were examined as a noninvasive biomarker of peripheral airway/alveolar  
34 inflammation.  $C_{ANO(TMAD)}$  and maximal NO flux in the airway compartment,  $J'_{awNO}$ ,  
35 were estimated with a model that incorporated trumpet shaped airways and axial  
36 diffusion using exhaled NO output at different flow rates. Measures of pulmonary  
37 function were then assessed by spirometry and an impulse oscillometry system, and  
38 their bronchodilator reversibility was examined. **Results:**  $C_{ANO(TMAD)}$  levels were not  
39 correlated with pre- or post-bronchodilator spirometric values, but were significantly  
40 associated with pre-bronchodilator reactance at low frequency ( $X_{rs5}$ ) ( $\rho=-0.31$ ,  
41  $p=0.011$ ), integrated area of low-frequency  $X_{rs}$  ( $AX$ ) ( $\rho=0.35$ ,  $p=0.003$ ) and negative  
42 frequency dependence of resistance ( $R_{rs5}-R_{rs20}$ ) ( $\rho=0.35$ ,  $p=0.004$ ). Furthermore,  
43  $C_{ANO(TMAD)}$  levels were associated with bronchodilator reversibility of  $FEV_1$ ,  $FEF_{25-75\%}$ ,  
44  $X_{rs5}$ , and  $AX$  ( $\rho=0.35$ ,  $\rho=0.31$ ,  $\rho=-0.24$ ,  $\rho=-0.31$ , respectively;  $p\leq 0.05$  for all).  
45 No variables were related to  $J'_{awNO}$ . **Conclusions:** Elevated  $C_{ANO(TMAD)}$ , but not  
46  $J'_{awNO}$ , partly reflects reversible airway obstruction originating in the peripheral airway.  
47 These findings indicate the involvement of peripheral airway inflammation in  
48 physiological abnormalities in asthma.

49

50 **Abbreviations**

51 AX: integrated area of low-frequency reactance

52 BD: bronchodilator

53 C<sub>ANO</sub>: alveolar fraction of exhaled NO

54 C<sub>ANO(TMAD)</sub>: alveolar fraction of exhaled NO adjusted for trumpet shaped airways and

55 axial diffusion

56 FEF<sub>25-75%</sub>: mid forced expiratory flow

57 FeNO: fraction of exhaled NO

58 FeNO<sub>50</sub>: FeNO at 50 ml/sec

59 ICS: inhaled corticosteroids

60 IOS: impulse oscillometry system

61 J'<sub>awNO</sub>: bronchial NO maximal flux adjusted for trumpet shaped airways and axial

62 diffusion

63 NO: nitric oxide

64 R<sub>rs</sub>: resistance of the total respiratory system

65 R<sub>rs5</sub>: R<sub>rs</sub> at 5 Hz

66 R<sub>rs20</sub>: R<sub>rs</sub> at 20 Hz

67 X<sub>rs</sub>: reactance of the total respiratory system

68 X<sub>rs5</sub>: X<sub>rs</sub> at 5 Hz

69

70 **Introduction**

71

72 Asthma is a chronic inflammatory disorder involving proximal airways as well as small  
73 peripheral airways [1-4]. Nitric oxide (NO) is a well-established noninvasive biomarker  
74 of inflammation in asthmatic airways [5]. Recently, the alveolar fraction of exhaled NO  
75 ( $C_{ANO}$ ) has been introduced to assess inflammation of peripheral airway/alveolar  
76 regions [6]. This variable has received renewed interest as a noninvasive tool for both  
77 adults [7] and children [8]. Although  $C_{ANO}$  is mathematically derived from NO output  
78 measured at multiple flow rates, a study by Berry and colleagues has shown a strong  
79 correlation between  $C_{ANO}$  levels and eosinophil counts in bronchoalveolar lavage fluid  
80 [9], suggesting that  $C_{ANO}$  may reflect peripheral airway/alveolar inflammation.  
81 Moreover, two trumpet models with axial diffusion have recently been developed to  
82 correct the effect of axial contamination by small airway NO diffusion on  $C_{ANO}$  [10, 11].  
83 This new parameter,  $C_{ANO(TMAD)}$ , precludes overestimating actual NO production in the  
84 alveolar region.

85         Peripheral airway dysfunction or the degree of air trapping is associated with  
86 recurrent exacerbations of severe asthma [12] or with disease severity [13]. Effective  
87 prevention of peripheral airway dysfunction requires an understanding of the  
88 contribution of peripheral airway inflammation to airway dysfunction. However, such a  
89 contribution has been confirmed only for severe refractory asthma [14, 15]. Because  
90 peripheral airway inflammation is not limited to patients with severe disease [1], we  
91 hypothesized that sustained inflammation in the peripheral airway or alveolar region  
92 may be linked to airway dysfunction in the general population of patients with asthma.  
93 In this study, we measured  $C_{ANO(TMAD)}$ , pulmonary function and pulmonary function

94 reversibility in response to treatment with a bronchodilator (BD) for patients with  
95 asthma ranging from mild intermittent to severe persistent. Using an impulse  
96 oscillometry system (IOS) [16] [17], we examined negative frequency dependence and  
97 low frequency reactance that could be proxies for peripheral airway function.

98

## 99 **Methods**

### 100 **Subjects**

101 This cross-sectional study was conducted at the outpatient asthma and cough  
102 clinic of Kyoto University Hospital from January through December 2007. We  
103 examined NO levels at different flow rates (50, 100, and 200 ml/s) in 75 adults with  
104 stable asthma. The inclusion criteria were as follows: 1) a diagnosis of asthma as  
105 defined by the American Thoracic Society [18] on the basis of a history of recurrent  
106 episodes of wheezing and chest tightness with or without cough; 2) confirmation of  
107 airway hyperresponsiveness on past evaluations; 3) regular attendance at our clinic for  
108 >3 months; 4) no exacerbation of asthma during the last 4 weeks; 5) no changes in  
109 treatment during the last 4 weeks; 6) non-smokers or ex-smokers who had smoked <10  
110 pack-years but had not smoked for >1 year; 7) no evidence of other respiratory diseases  
111 on chest X-ray findings. Severity was defined according to the step classification of the  
112 2004 version of the Global Initiative for Asthma guidelines [19]. Three patients with  
113 step 2 asthma were treated with leukotriene receptor antagonists because they refused to  
114 use inhaled corticosteroids (ICS). To examine patients with persistent airway  
115 inflammation, we measured NO levels at higher flows in patients with fraction of  
116 exhaled NO (FeNO) at 50 ml/sec (FeNO<sub>50</sub>) values  $\geq$  25 ppb [5]. The ethics committee  
117 of our institution approved the study protocol, and written informed consent was

118 obtained from each participant.

119

120 **Measurement of NO and calculation of  $C_{NO(TMAD)}$  and bronchial NO maximal**  
121 **flux**

122 NO levels were measured with a chemiluminescence analyzer (NOA 280,  
123 Sievers, Boulder, CO, USA) according to current guidelines, apart from the expiratory  
124 flow rate [20]. The analyzer was calibrated daily with gas without NO generated by  
125 exposing ambient air to NO scavengers and a standard concentration of 640 ppb NO.  
126 The lower detection limit for NO was 2 ppb. The signal output from the NO analyzer  
127 was fed to a computer data acquisition program, and concentrations were measured  
128 using a data analysis program (NOA Analysis™ Software, Sievers, Boulder, CO, USA).  
129 Seated subjects inserted a mouthpiece, inhaled orally to total lung capacity, exhaled  
130 immediately against a resistance, and maintained mouth pressure at 20 cmH<sub>2</sub>O,  
131 displayed on a pressure gauge. The steady-state NO plateau was taken as the FeNO  
132 value. By varying expiratory resistances, we measured FeNO levels at three expiratory  
133 flows of 50, 100 and 200 ml/s in that order. If an adequate NO plateau was not reached  
134 at 200 ml/s, patients were then instructed to exhale at a flow of 150 ml/s instead (n=4).

135  $C_{NO(TMAD)}$  was estimated using a model recently developed by Condorelli and  
136 colleagues that incorporated trumpet shaped airways and axial diffusion [10] rather than  
137 simply assuming that the lung was comprised of two separate regions with a rigid  
138 airway compartment and a well mixed expansible compartment [6]. The equation used  
139 was the following:  $C_{NO(TMAD)} = \text{slope} - \text{intercept}/740$ . The slope and intercept of this  
140 equation were determined from a linear regression line after plotting NO output (i.e.,  
141 exhaled NO level times expiratory flow) as a function of expiratory flow. When

142  $C_{ANO(TMAD)}$  values were  $<$  zero, they were assigned a value of zero. Bronchial NO  
143 maximal flux ( $J'_{awNO}$ ), a marker of inflammation in the airway compartment, was also  
144 determined by multiplying the intercept by 1.7. Because this trumpet model with axial  
145 diffusion was developed based on the assumption that NO flux from the airway tree was  
146 a constant and this simplified equation was valid at an expiratory flow rate between 100  
147 ml/s and 250 ml/s, we applied FeNO levels at 100 ml/s and 200 ml/s to obtain a linear  
148 regression line between NO output and exhalation flow. Five patients whose results had  
149 negative slopes were excluded from further analysis [10].

150

### 151 **Pulmonary function tests**

152 After NO measurements, subjects underwent pre- and post-BD (i.e., inhalation  
153 of 200  $\mu$ g salbutamol) pulmonary function testing. Respiratory impedance was  
154 measured by IOS followed by spirometric testing. Reversibility of the impedance and  
155 spirometric values was calculated by: (post-BD value minus pre-BD value)/pre-BD  
156 value.

157 Spirometry was performed according to the standards of the American Thoracic  
158 Society [21] using a ChestGraph HI-701 spirometer (Chest, Tokyo, Japan). FEV<sub>1</sub> and  
159 mid forced expiratory flow (FEF<sub>25-75%</sub>) were determined.

160 Respiratory impedance was measured using a Jaeger MasterScreen, IOS<sup>TM</sup>  
161 (Erich Jaeger, Hoechberg Germany) that met standard recommendations [22]. The IOS  
162 is different from the classical forced oscillation technique by the use of an impulse  
163 rather than a pseudorandom noise signal and in data processing. In brief, rectangular  
164 mechanical impulses containing a continuous power spectrum ranging from 0 to 100 Hz,  
165 generated by a loudspeaker at intervals of 0.2 s, were applied to the respiratory system

166 through a mouthpiece during tidal breathing. The resulting pressure and flow signals  
167 were measured next to the mouthpiece, and were analyzed for amplitude and phase  
168 differences using a fast Fourier transform to determine resistance (Rrs) and reactance  
169 (Xrs) of the total respiratory system. To reduce loss of energy in the upper airways, the  
170 chin and cheeks were supported by the subjects' hands. As proxies for peripheral airway  
171 function [16] [17] [23] [24], we used the negative frequency dependence of Rrs between  
172 5 and 20 Hz (Rrs5-Rrs20), Xrs at 5 Hz (Xrs5), and reactance area (AX) that is the  
173 integral of Xrs from 5 Hz to the resonant frequency at which Xrs crosses zero. Rrs at 20  
174 Hz (Rrs20) was used as a measure of proximal airway resistance, as oscillatory pressure  
175 components at frequencies  $\geq 20$  Hz are thought to be damped out before reaching the  
176 peripheral airways [16].

177

### 178 **Statistical analysis**

179 Data were analyzed using GraphPad Prism 4.00 (GraphPad Software, Inc., La Jolla, CA,  
180 USA) and StatView software 5.0 (SAS Institute Inc, Cary, NC, USA). When data were  
181 normally distributed, linear regression analysis was used. Otherwise, Spearman's rank-  
182 correlation test was used. The correlation coefficient from linear regression analysis is  
183 denoted as R, whereas Spearman's correlation coefficient is given as rho. Results are  
184 expressed as means  $\pm$  SDs or medians (ranges). We considered p values of  $\leq 0.05$  to  
185 indicate statistical significance.

186



187 **Results**

188 **Patients' characteristics**

189 The characteristics of the 70 subjects are shown in Table 1. Measures of pulmonary  
190 function and FeNO<sub>50</sub> of the 70 subjects did not differ significantly from those of the 5  
191 patients whose slopes were negative (data not shown).

192

193 **Correlations between patients' characteristics and C<sub>ANO(TMAD)</sub> or bronchial flux**

194 Patients with more severe asthma showed a trend for higher J'<sub>awNO</sub> levels than those  
195 with milder disease ( $\rho=0.23$ ,  $p=0.056$ ), but not for C<sub>ANO(TMAD)</sub> levels ( $\rho=0.17$ ,  
196  $p=0.17$ ). The presence of atopy, rhinitis and smoking history were not associated with  
197 C<sub>ANO(TMAD)</sub> or J'<sub>awNO</sub> (data not shown).

198

199 **Correlations of C<sub>ANO(TMAD)</sub> or bronchial flux with pre- and post-BD pulmonary**  
200 **function measures**

201 The associations of C<sub>ANO(TMAD)</sub> and J'<sub>awNO</sub> with pulmonary function measures are  
202 summarized in Table 2. Correlations of pulmonary function measures with FeNO<sub>50</sub> that  
203 were strongly correlated with J'<sub>awNO</sub> levels ( $\rho=0.83$ ,  $p<0.0001$ ) are also shown in this  
204 table. There was no association of C<sub>ANO(TMAD)</sub> with pre-BD %FEV<sub>1</sub>, %FEF<sub>25-75%</sub>, or  
205 Rrs20. C<sub>ANO(TMAD)</sub> was significantly associated with pre-BD Rrs5-Rrs20, Xrs5, and AX  
206 (Fig 1). The association between Xrs5 and C<sub>ANO(TMAD)</sub> remained significant even when  
207 two obvious outliers (one with the highest Xrs5 and another with the lowest Xrs5) were  
208 excluded ( $\rho=-0.36$ ,  $p=0.003$   $n=68$ ). There was no association between C<sub>ANO(TMAD)</sub> and  
209 any measure of post-BD pulmonary function. J'<sub>awNO</sub> was not related to any indices of  
210 pulmonary function.

211 Measures of pre-BD Rrs5-Rrs20, Xrs5, and AX were moderately to strongly  
212 correlated with each other ( $|\rho|$  ranged between 0.75 and 0.93,  $p < 0.0001$ ). These  
213 measures of pre-BD IOS were correlated with pre-BD %FEV<sub>1</sub> ( $|\rho|$  ranged between  
214 0.33 and 0.40,  $p < 0.01$ ).

215

216 **Correlations between C<sub>ANO(TMAD)</sub> or bronchial flux and reversibility of pulmonary**  
217 **function measures**

218 Reversibilities of FEV<sub>1</sub> and FEF<sub>25-75%</sub>, as well as of Xrs5 and AX, were significantly  
219 associated with C<sub>ANO(TMAD)</sub> (Table 2). J'awNO was not related to any indices of  
220 reversibility.

221 Reversibilities of FEV<sub>1</sub>, FEF<sub>25-75%</sub> Xrs5 and AX were associated with pre-BD  
222 levels; reversibility of FEV<sub>1</sub> was correlated with the pre-BD FEV<sub>1</sub> level ( $R = -0.56$ ,  
223  $p < 0.0001$ ); for %FEF<sub>25-75%</sub>,  $\rho = -0.25$ ,  $p = 0.042$ ; for Xrs5,  $\rho = 0.48$ ,  $p < 0.0001$ ; for AX,  
224  $\rho = -0.40$ ,  $p = 0.001$ .

225

226

227 **Discussion**

228 To the best of our knowledge, this is the first study to demonstrate that in adult patients  
229 with stable asthma,  $C_{ANO(TMAD)}$ , but not  $J'_{awNO}$ , is significantly associated with Rrs5-  
230 Rrs20, Xrs5, and AX levels, which are thought to reflect peripheral airway function.  
231 Our novel findings are that the increase in  $C_{ANO(TMAD)}$  associates with greater  
232 reversibility of FEV<sub>1</sub>, FEF<sub>25-75%</sub>, Xrs5 and AX in response to treatment with a BD.  
233 These findings suggest that peripheral airway/alveolar inflammation may contribute to  
234 reversible airway obstruction originating in the peripheral airway.

235 Before the introduction of  $C_{ANO(TMAD)}$ ,  $C_{ANO}$  had been used as a reasonably well  
236 validated marker of inflammation of the peripheral airway/alveolar region [9].  
237 Histological studies have suggested that peripheral airway inflammation has a similar or  
238 greater impact on disease severity than does proximal airway inflammation [1, 23, 24].  
239 Studies examining  $C_{ANO}$  have drawn similar conclusions;  $C_{ANO}$  in refractory asthma is  
240 significantly greater than that in mild to moderate asthma [9], and patients with oral  
241 steroid-dependent asthma have higher  $C_{ANO}$  levels than patients with mild-to-moderate  
242 or severe asthma [14] [25]. In this study,  $J'_{awNO}$  showed a trend toward increased  
243 values in patients with more severe asthma than those with milder disease. However,  
244 when  $C_{ANO(TMAD)}$  was determined using a trumpet model with axial diffusion that  
245 estimated NO concentrations exiting the respiratory bronchioles and alveolar region,  
246  $C_{ANO(TMAD)}$  was not correlated with disease severity, which is consistent with a recent  
247 finding by Mahut et al [26]. Given that  $C_{ANO}$  is not adjusted for NO axial diffusion  
248 from conducting airways and could be more contaminated by small airway NO  
249 diffusion than  $C_{ANO(TMAD)}$ , this discrepancy between previous findings with  $C_{ANO}$  and  
250 those with  $C_{ANO(TMAD)}$  in this study may indicate that small airway inflammation

251 influences asthma severity to a greater extent than the actual alveolar inflammation.  
252 Indeed, a histological study of severe asthmatics showed that small airways with  
253 perimeters less than 6 mm were the most significantly infiltrated by inflammatory cells  
254 across the entire airway tree, from the large airways to the alveolar tissue [23].

255 Van Veen and colleagues found significant correlations of  $C_{ANO}$  with  
256 peripheral airway obstruction, as assessed by residual volume, functional residual  
257 capacity and closing capacity [14], in patients with severe asthma. However, when  
258 patients with mild-to-moderate asthma were included, these correlations disappeared,  
259 and only a significant association between  $C_{ANO}$  and the slope of the single breath  
260 nitrogen washout curve remained. Although  $C_{ANO}$  was correlated with  $FEF_{25-75\%}$  in  
261 children with refractory asthma [15],  $C_{ANO}$  was not correlated with  $FEF_{50\%}$ ,  $FEF_{25\%}$ , or  
262 residual volume in adults with asthma [25]. These studies provide little or no evidence  
263 of a link between peripheral airway inflammation and dysfunction in the population of  
264 adults with asthma.

265 In the current study, however,  $C_{ANO(TMAD)}$  was modestly, but significantly  
266 associated with small airway reactance/capacitance ( $X_{rs5}$ ,  $AX$ ) and negative frequency  
267 dependence of airway resistance ( $R_{rs5}$ - $R_{rs20}$ ). These variables obtained by IOS, a non-  
268 invasive and effort-independent tool, have been proposed as relevant and sensitive  
269 indices of peripheral airway function [16] [17] [23] [28] [27] [28]. Previous oscillation  
270 studies have demonstrated that as peripheral resistance increases, the resistance at low  
271 frequencies increases compared to the higher frequencies, thereby resulting in greater  
272 negative frequency dependence of  $R_{rs}$  [16, 29].  $X_{rs}$  at low frequency is also considered  
273 to reflect the capacitative properties of peripheral airways and to detect peripheral  
274 airway narrowing [30]. In our recent study of patients with asthma,  $R_{rs5}$ - $R_{rs20}$  and  $AX$ ,

275 but not Rrs20, are significantly associated with residual volume [23]. Another recent  
276 long-term study of controller therapy for pediatric asthma also demonstrates that AX  
277 may be sensitive to changes in peripheral airway function [27]. The nature of these  
278 indices of IOS may support our premise that Rrs5-Rrs20, Xrs, and, particularly, AX  
279 may reflect peripheral airway function. However, as discussed below, the data should be  
280 interpreted with caution because IOS indices are indirect measures, and no associations  
281 of IOS indices with pathological changes have been demonstrated thus far.

282         Airway variability is another feature of asthma, implying instability of the  
283 disease. Endobronchial and transbronchial biopsy studies of nocturnal asthma have  
284 demonstrated a significant contribution of peripheral airway inflammation to nocturnal  
285 decrement of pulmonary function as compared with proximal airway inflammation [31].  
286 In studies of pediatric asthma, higher FeNO levels are associated with greater FEV<sub>1</sub>  
287 reversibility [32-34]. Tsuburai and colleagues show associations between FeNO levels  
288 and FEV<sub>1</sub> reversibility in adult asthmatics with airflow limitation, but not in those  
289 without airflow limitation [35]. Our study of adult asthmatics extended the previous  
290 findings by showing that smoldering inflammation in the peripheral airway/alveolar  
291 compartment is responsible for greater BD response in FEV<sub>1</sub>, FEF<sub>25-75%</sub>, Xrs5, and AX,  
292 and that reversibility to a BD depends on the degree of pre-BD obstruction. Given that  
293 C<sub>ANO(TMAD)</sub> was correlated with pre-BD Xrs5 and AX, but not with FEV<sub>1</sub> or FEF<sub>25-75%</sub>  
294 values, we speculate that peripheral airway/alveolar inflammation may contribute to  
295 reversible airway obstruction originating in the peripheral airway.

296         In sharp contrast to C<sub>ANO(TMAD)</sub>, bronchial NO flux (i.e. J<sub>awNO</sub> levels) was not  
297 correlated with any indices of pulmonary function and FeNO<sub>50</sub> was only correlated with  
298 reversibility of Xrs5, which was consistent with other studies [7] [36]. This discrepancy

299 between  $C_{ANO(TMAD)}$  and  $J'_{awNO}$  could be attributed to differences in their responses to  
300 ICS treatment. When patients are treated with an ICS,  $J'_{awNO}$  readily decreases,  
301 whereas  $C_{ANO}$  is resistant to them [37]. Therefore, we speculate that any correlation of  
302  $J'_{awNO}$  or  $FeNO_{50}$  with pulmonary function might have been modified by ICS treatment.  
303 Indeed, in steroid naïve patients, exhaled NO levels are correlated with airway  
304 hyperresponsiveness [38], asthma symptom scores [39], or with bronchodilator response  
305 [34], whereas such correlations disappear in patients on ICS. Intriguingly, a recent study  
306 shows significant associations between exhaled NO levels and  $FEV_1$  or bronchodilator  
307 responses in pediatric asthmatics receiving ICS treatments when they are classified  
308 according to their ICS doses [40], which may suggest that stratifying patients by ICS  
309 doses could provide deeper insights into the roles of exhaled NO in patients on ICS.

310         The role of  $C_{ANO(TMAD)}$  in peripheral airway obstruction should not be  
311 overestimated because the associations were modest; elevated  $C_{ANO(TMAD)}$  is not a  
312 strong indicator for low  $Xrs5$  or increased  $AX$ . Also, IOS variables were not compared  
313 with closing volume or closing capacity, other proxy measures of peripheral airway  
314 obstruction. As mentioned above, IOS measurements have several limitations and  
315 should be interpreted cautiously [16] [17] because of issues that include artifact effects  
316 of upper airway compliance and leaks at the mouthpiece. Increases in  $Rrs5$ - $Rrs20$  may  
317 imply heterogeneity of peripheral airway narrowing in addition to an absolute increase  
318 in resistance [41].  $Xrs5$  is relatively noise-sensitive, whereas  $AX$  is less so. Resistance  
319 and reactance in the peripheral airway may indicate different properties, given that pre-  
320 BD values of  $Rrs5$ - $Rrs20$  were not correlated with reversibility to a BD, whereas pre-  
321 BD values of  $AX$  and  $Xrs5$  were, although precise mechanisms underlying this  
322 discrepancy are unknown.

323           We may have missed some patients with normal FeNO<sub>50</sub> and high C<sub>ANO(TMAD)</sub>  
324 by excluding those with FeNO<sub>50</sub> < 25 ppb. When pediatric patients with asthma are  
325 grouped based on their J'<sub>awNO</sub> and C<sub>ANO(TMAD)</sub> levels, Puckett et al find that 11% of the  
326 patients have normal J'<sub>awNO</sub> and high C<sub>ANO(TMAD)</sub> levels [42]. However, when we  
327 examined another 21 patients with stable asthma who had FeNO<sub>50</sub> < 25 ppb, their ratios  
328 of C<sub>ANO(TMAD)</sub> levels to FeNO<sub>50</sub> levels did not differ from those of the currently studied  
329 population (data not shown), suggesting that patients with normal FeNO<sub>50</sub> and high  
330 C<sub>ANO(TMAD)</sub> are not commonly observed in our patient population. Therefore, we believe  
331 that the possibility of missing patients with normal FeNO<sub>50</sub> and high C<sub>ANO(TMAD)</sub> may  
332 not have severely affected our findings.

333           Five patients were excluded from the analysis because their results had  
334 negative slopes in plots of NO output vs. expiratory flow between 100 ml/s and 200  
335 ml/s. NO axial diffusion from the airway tree increases as bronchial flux increases and  
336 its relative impact over NO conductive transport exiting the alveolar region is greater at  
337 lower expiratory flows [10]. Therefore, the negative slopes for five patients may  
338 indicate that, in these patients, the relative impact of NO axial diffusion on NO output  
339 with exhalation flows around 100 ml/s might have remained either because of increased  
340 bronchial reflux or because of relatively small NO production in the alveolar region.  
341 Measurements with higher expiratory flows would have been desirable, but it was  
342 difficult for our patients to obtain a steady-state NO plateau with higher flows, such as  
343 at 250 ml/s or 300 ml/s. Despite these limitations, our findings support the superiority of  
344 a multiple flow technique to a conventional single flow measurement, as the former  
345 provides information on peripheral airway/alveolar inflammation.

346           In conclusion, inflammation in the peripheral airway/alveolar region as

347 assessed by CANO(TMAD) partly contributes to the development of peripheral airway  
348 obstruction and to reversibility of pulmonary function in response to a bronchodilator.  
349 Monitoring peripheral airway/alveolar inflammation may provide higher-quality  
350 information for patients with asthma.

351

352



353 **The authors have no conflicts of interest to disclose.**

354

355

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484

485 **Figure legend**

486 Figure 1. Relationships between  $C_{ANO(TMAD)}$  levels and pre-bronchodilator Xrs5 (left)  
487 and Rrs5-Rrs20 (right).

488



489 Table 1. Patients' characteristics (n=70)

490	Gender, M/F	33/37
491	Age, yr	57.4 ±15.6
492	Disease duration, yr	12.2 ± 10.4
493	Asthma severity*, 1/2/3/4	2/35/17/16
494	Atopy, positive <sup>†</sup> , %	66
495	IgE, IU	190 (5, 6800)
496	Ex smoker, %	33
497	Sinusitis/rhinitis, %	66
498	Daily dose of ICS <sup>‡</sup> , µg	400 (0, 1600)
499	%FEV <sub>1</sub> , %	89.4 ± 16.5
500	%FEF <sub>25-75%</sub> , %	57.4 ± 26.8
501	Rrs <sub>20</sub> , kPa·s·L <sup>-1</sup>	0.32 ± 0.11
502	Rrs <sub>5</sub> -Rrs <sub>20</sub> , kPa·s·L <sup>-1</sup>	0.06 (-0.03, 0.43)
503	Xrs <sub>5</sub> , kPa·s·L <sup>-1</sup>	-0.13 (-0.56, 0.17)
504	AX, kPa·s·L <sup>-1</sup>	0.44 (0.01, 5.51)
505	FeNO <sub>50</sub> , ppb	44.9 (25.0, 224.4)
506	J' <sub>aw</sub> NO, pl·s <sup>-1</sup>	3638 (0, 15300)
507	CANO <sub>(TMAD)</sub> , ppb	3.9 (0, 34.9)

508

509 \*According to the Global Initiative for Asthma guidelines [19]. <sup>†</sup>Considered atopic  
 510 when one or more specific IgE antibodies against house dust mite, cat dander, dog  
 511 dander, molds, weed, cedar pollen, or grass pollen were positive. <sup>‡</sup>Equivalent dose of  
 512 fluticasone. ICS = inhaled corticosteroids, Rrs<sub>20</sub> = resistance of the total respiratory  
 513 system at 20 Hz, Rrs<sub>5</sub> = Rrs at 5 Hz, Xrs<sub>5</sub> = reactance at 5 Hz, AX = area of low-  
 514 frequency reactance, FeNO<sub>50</sub> = exhaled NO level at flow of 50 ml/s, J'<sub>aw</sub>NO = bronchial  
 515 NO maximal flux adjusted for trumpet shaped airways and axial diffusion, CANO<sub>(TMAD)</sub>  
 516 = alveolar fraction of exhaled NO adjusted for trumpet shaped airways and axial  
 517 diffusion

518 Values are means ± SD or median (range).

519

520 Table 2. Correlation coefficients of NO levels with pulmonary function values

521		CANO(TMAD)	J'awNO	FeNO <sub>50</sub>
522	Pre-bronchodilator			
523	%FEV <sub>1</sub>	-0.18	-0.03	-0.12
524	%FEF <sub>25-75%</sub>	-0.09	-0.05	-0.10
525	Rrs20	0.22	-0.17	-0.05
526	Rrs5-Rrs20	<b>0.35<sup>†</sup></b>	-0.09	0.11
527	Xrs5	<b>-0.31*</b>	-0.05	-0.19
528	AX	<b>0.35<sup>†</sup></b>	-0.03	0.14
529	Reversibility			
530	ΔFEV <sub>1</sub>	<b>0.35<sup>†</sup></b>	-0.007	0.09
531	ΔFEF <sub>25-75%</sub>	<b>0.31*</b>	0.09	0.21
532	ΔRrs20	-0.23	-0.007	-0.01
533	Δ(Rrs5-Rrs20)	-0.22	0.05	0.01
534	ΔXrs5	<b>-0.24*</b>	-0.16	<b>-0.25*</b>
535	ΔAX	<b>-0.31*</b>	-0.16	-0.10

536 \*:  $p \leq 0.05$ , <sup>†</sup>:  $p < 0.01$ , Correlation coefficients of Spearman's correlation coefficients  
 537 are shown.

538  $\Delta = (\text{post-bronchodilator value minus pre-bronchodilator value}) / \text{pre-bronchodilator}$   
 539 value, Rrs20 = resistance of the total respiratory system at 20 Hz, Rrs5 = Rrs at 5 Hz

540 Xrs5 = reactance at 5 Hz, AX = integrated area of low-frequency reactance,

541 C<sub>ANO(TMAD)</sub> = alveolar fraction of exhaled NO adjusted for trumpet shaped airways and

542 axial diffusion, J'awNO = bronchial NO maximal flux adjusted for trumpet shaped

543 airways and axial diffusion, FeNO<sub>50</sub> = fraction of exhaled NO at 50 ml/sec

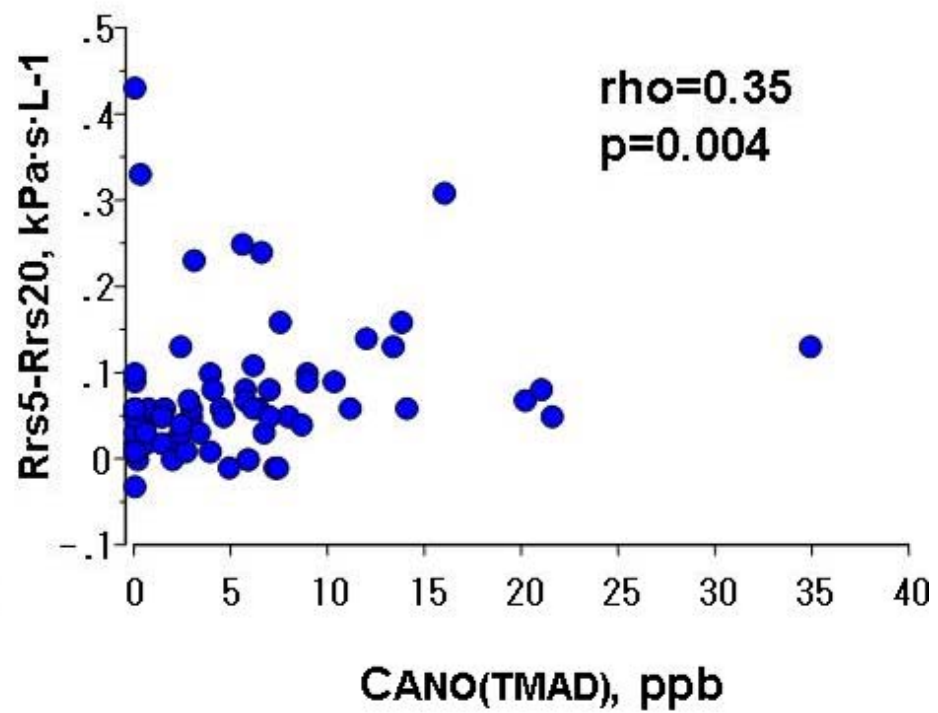
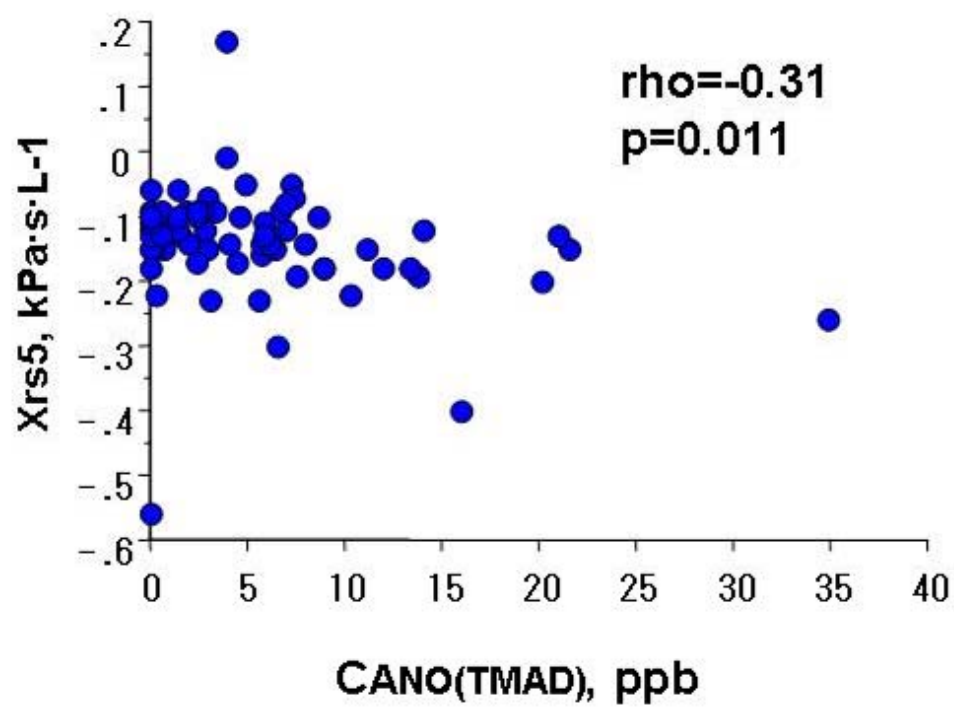


Figure 1