

1   **Title**

2   Diagnostic Performance between Contrast Enhancement, Proton MR Spectroscopy and

3   Amide Proton Transfer Imaging in Patients with Brain Tumors

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## ABSTRACT

### Purpose

To explore the relationship among parameters of magnetic resonance spectroscopy (MRS) and amide proton transfer (APT) imaging, and to assess the diagnostic performance of MRS and APT imaging for grading brain tumors in comparison with contrast enhancement of conventional MRI for preoperative grading in patients with brain tumor.

### Materials and Methods

Institutional review board approval and written informed consent were obtained. Forty-one patients with suspected brain tumors were enrolled in the study. Single-voxel MRS and two-dimensional APT imaging of the same slice level were conducted using a 3-T MRI scanner. Positive or negative contrast enhancement on T1-weighted images was assessed by two neuroradiologists. Correlations among metabolite concentrations, metabolite ratios, and calculated histogram parameters, including mean APT ( $APT_{mean}$ ) and the 90th percentile of APT ( $APT_{90}$ ) were assessed using Spearman's correlation coefficient. Diagnostic performance was evaluated with receiver operating characteristic (ROC) curve analysis for contrast enhancement, MRS and APT imaging. Values of  $p < 0.05$  were considered statistically significant.

## Results

Positive correlations with statistical significance were found between total concentration of Cho and APT<sub>90</sub> ( $r=0.49$ ), and between Cho/Cr and APT<sub>mean</sub> ( $r=0.65$ ) as well as APT<sub>90</sub> ( $r=0.49$ ). A negative correlation with statistical significance was observed between NAA/Cr and APT<sub>mean</sub> ( $r=-0.52$ ). According to ROC curves, Cho/Cr, APT<sub>mean</sub>, APT<sub>90</sub>, demonstrated higher AUC values than that of contrast enhancement in grading gliomas.

## Conclusions

Significant correlations were observed between metabolite concentrations and ratios on MRS and APT values. MRS and APT imaging showed comparable diagnostic capability for grading brain tumors, suggesting that both MRS and APT imaging offer potential for quantitatively assessing similar biological characteristics in brain tumors on non-contrast MRI.

## Key Words

Amide proton transfer imaging;  
Chemical exchange saturation transfer;  
Magnetic Resonance Imaging;

1 Magnetic Resonance Spectroscopy;

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1  
2       Conventional magnetic resonance imaging (MRI) with gadolinium-based  
3 contrast agent has been accepted as a standard method for the characterization of brain  
4 tumors. In particular, disruption of the blood-brain barrier (BBB) as observed on  
5 contrast enhanced (CE) T1-weighted imaging is used as a measure of brain tumor  
6 malignancy and grading.<sup>1</sup> However, the accuracy of this approach is reportedly  
7 limited.<sup>2,3</sup> Moreover, with the recent availability of anti-angiogenic pharmacotherapies  
8 such as bevacizumab and other agents,<sup>4,5</sup> evaluating the status of brain tumors has been  
9 complicated by the protection of the BBB afforded by these treatment.<sup>6</sup>

10       Several studies have investigated the visualization and characterization of brain  
11 tumors without using contrast media. Among these, <sup>1</sup>H-magnetic resonance  
12 spectroscopy (MRS) has been established as a technique providing information on  
13 chemical metabolites present in living tissues.<sup>7</sup> Amide proton transfer (APT) imaging, a  
14 novel chemical exchange saturation transfer (CEST)-based molecular MRI technique,  
15 has recently been introduced to the clinical setting.<sup>8-12</sup> APT imaging is designed to  
16 detect endogenous mobile proteins and peptides in tissues.<sup>13</sup> Both MRS and APT  
17 imaging provide metabolic information that can be exploited to study the biological  
18 behaviors of tumors.<sup>14,15</sup>

We assumed that APT imaging and metabolites identified on MRS would show similarities and correlations and would provide important oncologic information. To date, several studies have demonstrated that these advanced techniques have the potential to characterize brain tumors.<sup>7-12,16-18</sup> However, very few clinical studies have discussed correlations between findings from MRS and APT imaging.<sup>19</sup>

The objectives of this study were to: 1) explore relationships among parameters obtained from MRS and APT imaging and 2) assess the diagnostic performance of APT imaging and MRS for grading brain tumors in comparison with contrast enhancement of conventional MRI.

## **MATERIALS AND METHODS**

### ***Patients***

The institutional review board of our university approved this study. Written informed consent was obtained from all patients or their guardian/s. Between May 2013 and August 2014, a total of 41 consecutive patients with suspected brain tumor and symptoms corresponding to World Health Organization (WHO) performance status  $\leq 2$  were enrolled in the study. The following inclusion criteria were used: a) MRS and APT imaging performed during the same examination; and b) presence of treatment-naïve or

recurrent tumor with histological verification. Exclusion criteria were: a) degradation of image quality due to susceptibility artifacts or motion artifacts; b) unsatisfactory shimming such as a larger full width at half maximum (FWHM) of water peak reaching  $>0.10$  ppm; or c) extra-axial tumors such as meningioma. When motion artifacts were suspected, original series of APT imaging were visually inspected if there are apparent movements of head position during image acquisition. Five patients were excluded due to severe motion artifacts during APT imaging (a), 5 patients were excluded due to the FWHM criterion (b), and 4 patients with lymphoma, one patient with brain metastasis from melanoma, 5 patients with meningioma were also excluded (c). A final total of 21 patients were thus included in this study.

## **MR Imaging**

### **MR Spectroscopy**

All MRI was performed using a whole-body 3-T system (Vantage; Toshiba Medical Systems, Otawara, Japan) with a 32-channel head coil. MRS was obtained using a single-voxel point-resolved spectroscopic sequence with water suppression pulse and the following parameters: repetition time (TR), 2000 ms; echo time (TE), 136 ms; flip angle,  $90^\circ$ ; and scan time, 4 min 18 s. The volume of interest (VOI) was placed

on the area showing the solid portion of tumor on T2-weighted imaging, and the cystic or necrotic portion and hemorrhagic regions were carefully avoided. Size of the VOI varied from  $15 \times 15 \times 15 \text{ mm}^3$  to  $20 \times 20 \times 20 \text{ mm}^3$ , depending on tumor size.

MR data were transferred to a workstation, then MRS was analyzed using LCModel version 6.3-0C software (LCModel, Ontario, Canada) using the basis set. Analysis was undertaken on water-suppressed spectral domain data for chemical shifts in the range of 0.0 - 4.0 ppm. Absolute concentrations of N-acetyl aspartate (NAA), creatine (Cr) and choline (Cho), and NAA to creatine ratio (NAA/Cr) and choline to creatine (Cho/Cr) ratios were calculated using known concentrations of tissue water.<sup>20</sup>

### *APT imaging*

APT imaging was conducted with a 2-dimensional fast advanced spin echo sequence, which is similar to the half-Fourier acquisition single-shot turbo spin-echo sequence. The imaging slice was set at the midpoint of the VOI of MRS, which enabled values of APT to be obtained at the VOI of MRS. The following parameters were used in a single-slice axial acquisition: field of view,  $230 \times 230 \text{ mm}$ ; matrix,  $256 \times 256$ ; TR, 9000 ms; TE, 60 ms; flip angle,  $90^\circ$ ; refocusing flip angle,  $160^\circ$ ; slice thickness, 5mm;

bandwidth, 651 Hz/pixel; saturation power, flip angle  $500^\circ$  (1  $\mu$ T); magnetization-transfer (MT) Contrast pulse shot, 25; inter-pulse delay, 1 ms; and scan time, 6 min 9 s. MT spectra over an offset range of  $\pm 10$  ppm with a step size of 0.5 ppm with respect to water resonance were obtained.

## ***Imaging Analysis***

### *Conventional MRI*

Two board-certified neuroradiologists (\_\_\_ and \_\_\_, with 8 and 17 years of experience) independently analyzed imaging characteristics of brain tumor. They assessed if contrast enhancement is present (CE +ve) or not (CE -ve) on CE T1-weighted image of patients with brain tumor.

### *APT imaging*

The minimum value for MT spectra obtained from APT imaging was estimated from the original data by spline interpolation with Lorentzian function fitting, and displacement from the water resonance frequency owing to B0-field inhomogeneity was corrected. For quantification, asymmetric magnetization transfer ratio ( $MTR_{\text{asym}}$ ) analysis was performed with respect to the water resonance frequency on the

1 shift-corrected z-spectrum fit between a parameter for amide proton exchange and its  
 2 symmetrically opposite side, such that  $MTR_{\text{asym}}(+\Delta\omega) = MTR(-\Delta\omega) - MTR(+\Delta\omega)$ ,  
 3 where MTR is the magnetization transfer ratio and  $\Delta\omega$  is the frequency (in parts per  
 4 million) of amide and the water exchange site with respect to water (typically between  
 5 3.3 and 3.7 ppm) obtained from the shift-corrected z-spectrum. The VOI of MRS was  
 6 automatically transferred to the APT image of each patient using an in-house script in  
 7 Matlab 2013b (The MathWorks, Natick, MA) (Fig. 1). Finally, mean  $MTR_{\text{asym}}$   
 8 ( $APT_{\text{mean}}$ ), the 90th percentile of  $MTR_{\text{asym}}$  ( $APT_{90}$ ), standard deviation, kurtosis and  
 9 skewness of VOIs were calculated.

### 11 ***Histologic Evaluation***

12 Pathological diagnosis was determined according to WHO 2007 criteria by a  
 13 board-certified neuropathologist.<sup>21</sup> Grade 1 and 2 were regarded as low grade, while  
 14 grade 3 and 4 were regarded as high grade.

### 16 ***Statistical Analysis***

17 Data were checked by Gaussian distribution and homogeneity testing before  
 18 analysis. Intra-rater agreements were assessed with Cohen's kappa. If there were

disagreement between the two raters, third radiologist (\_\_\_, a board-certified neuroradiologist with 24 years of experience) made final decision. Correlations between parameters obtained from MRS and APT imaging were analyzed using Spearman correlation analysis. Receiver-operating characteristic (ROC) analyses were conducted to determine optimal thresholds, as well as sensitivity and specificity for grading brain tumors with each technique. We used conventional MRI characteristics as reference standards. Areas under the curve (AUCs) were statistically compared using a method described by Delong et al.<sup>22</sup>

All statistical analyses were conducted using Stata version 13 software (Stata Corp, Texas, US). Values of  $p < 0.05$  were considered statistically significant.

## RESULTS

### *Patients*

Patient population was summarized in Table 1. Patients comprised 13 males and 8 females (mean age,  $50.0 \pm 20.2$  years; range, 11–85 years). Tumors comprised 21 gliomas (grade II, n=10; grade III, n=3; grade IV, n=8). Two patients were diagnosed with recurrent gliomas. Typical cases are shown in Fig. 1 and Fig. 2.

### ***Intra-rater agreement of conventional MRI analyses by neuroradiologists***

CE +ve was diagnosed in 16 patients, and CE -ve was diagnosed in 5 patients (Table 1). Cohen's kappa was 1.0 and agreement was 100%.

### ***Correlations between MRS and APT imaging***

Correlations between among metabolites concentration or ratio from MRS and APT<sub>mean</sub> or APT<sub>90</sub> are summarized in Table 2. Positive correlations with statistical significance were found between Cho and APT<sub>90</sub>, and between Cho/Cr and APT<sub>mean</sub>. Negative correlations with statistical significance were observed between NAA/Cr and APT<sub>mean</sub>. Negative correlations were observed between NAA and APT<sub>mean</sub> ( $r = -0.43$ ,  $p = 0.05$ ). Standard deviation, skewness and kurtosis of APT<sub>asym</sub> showed no significant correlations with Cho, NAA Cr, or its ratios (Table. 2).

### ***Diagnostic capability for grading brain tumors on contrast enhancement, MRS and APT imaging***

ROC curves illustrating the performance of contrast enhancement, Cho, Cho/Cr, APT<sub>mean</sub>, APT<sub>90</sub> are shown in Fig. 3. According to ROC curves, the APT<sub>mean</sub> cutoff of 2.72 offered the best combination of sensitivity (72.7%) and specificity (90%) in the

1 characterization of high-grade gliomas, while the APT<sub>90</sub> cut-off of 6.61 demonstrated  
 2 the optimal combination of sensitivity (90.9%) and specificity (70%).

3 Total concentration of Cho cutoff of 2.85 provided the best combination of  
 4 sensitivity (63.6%) and specificity (100%) among total concentration of metabolites.

5 Among the ratios of the two metabolites above, the Cho/Cr threshold value of 0.50  
 6 generated the best combination of sensitivity (100%) and specificity (93.8%) in the

7 discrimination of high- and low-grade tumors. AUCs of each parameter were

8 summarized in Table. 3. All the imaging parameters above except Cho demonstrated

9 higher AUC values than that of contrast enhancement (AUC was 0.65). None of the

10 AUCs obtained from these variables showed significant differences (Fig. 3, APT<sub>90</sub> vs

11 APT<sub>mean</sub>, P=0.74, APT<sub>90</sub> vs Cho/Cr, P=0.35, Cho/Cr vs APT<sub>mean</sub>, P=0.72).

## 13 DISCUSSION

14 We made two important observations in this study. First, we found significant

15 moderate correlations between the concentration of metabolites and APT<sub>asym</sub> parameters.

16 Few studies have investigated the associations among MRS and CEST. In the literature,

17 lactate and MTR<sub>asym</sub> at 3.5 ppm correlated well with infarcted area in induced middle

18 cerebral artery occlusion,<sup>23</sup> and a good correlation was seen between CEST at 2 ppm

and creatine concentration for implanted gliosarcoma cells.<sup>24</sup> However, those studies used rat models, and only one clinical study has investigated correlations between MRS and CEST in human brain tumors.<sup>19</sup> Some investigators prefer APT<sub>90</sub> or other variables close to maximum values over mean APT values,<sup>8,19</sup> because the 90% histogram cutoff is less influenced by random statistical fluctuations, and is thus considered superior to the maximum value.<sup>25</sup> When comparing Cho and APT<sub>90</sub>, a positive correlation was seen in patients with intra-axial brain tumors, supporting the recent results from Park et al.<sup>19</sup> These findings suggest the feasibility of quantitatively assessing similar biological characteristics in brain tumors using MRS and APT imaging as different modalities. Such correlation is unlikely to be due to signals from Cho, because the CEST effect at 3.5 ppm from endogenous metabolites including Cho and NAA might not be visible at 3T.<sup>26</sup> Generally, malignant tumor cells show high proliferative activity and cellularity. The Cho peak corresponds to increased cell attenuation and membrane turnover in neoplastic tissues.<sup>27,28</sup> APT values have recently been reported to show moderate correlations with cell density or MIB-1 index, as a representative marker for proliferative activity of the brain tumor.<sup>9</sup> A possible explanation for the positive correlation between Cho and APT<sub>90</sub>, therefore, involves the proliferative activity and cellularity of tumor cells.

1           We also found a negative correlation between NAA and  $APT_{mean}$ . NAA is  
2   predominantly located in neurons and is thus decreased in all neoplasms that cause  
3   neurons to be displaced or replaced with malignant cells.<sup>29</sup> Numerous studies have  
4   demonstrated decreased NAA peak, mainly in glial neoplasms<sup>30</sup> and primary CNS  
5   lymphoma,<sup>31</sup> consistent with our results. Our results also suggest that  $APT_{mean}$  indirectly  
6   reflects neuronal loss due to brain tumor infiltration. To testify our hypothesis, further  
7   study including stereotactic biopsy based on the APT image should be needed.

8           Interestingly, we neither found a positive correlation between Cho and  $APT_{mean}$ ,  
9   nor between NAA and  $APT_{90}$ . A possible explanation for this discrepancy is that  $APT_{90}$   
10   and  $APT_{mean}$  may be different biomarkers, and similar discrepancies were reported  
11   between minimum and mean apparent diffusion coefficient from diffusion-weighted  
12   imaging.<sup>32</sup> Jiang et al. recently showed that the maximum value from APT imaging was  
13   significantly lower in patients with primary CNS lymphoma than in patients with  
14   Glioblastoma, while  $APT_{mean}$  values did not show any such significant differences  
15   between patient groups.<sup>12</sup> To clarify and verify different information for these  
16   parameters, further studies are needed.

17           Second, MRS and APT imaging showed comparable diagnostic performance in  
18   differentiating between high- and low-grade brain tumors. Several studies have shown a

significant increase in Cho/Cr in high-grade tumors compared with that of low-grade tumors at long TE with clinical scanners.<sup>17,18</sup> Past studies also demonstrated that the utility of amount of metabolite or metabolite concentration ratio in grading brain tumor.<sup>33</sup> Recently, APT<sub>asym</sub> values are reportedly suitable for differentiating between high- and low-grade brain tumors, mainly in adult populations.<sup>8-11</sup> The diagnostic capability of MRS and APT imaging for grading brain tumors was investigated and compared with that of conventional MRI in this study. We found that MRS and APT imaging shows higher AUCs compared with that of grading diagnosed by neuroradiologists based on conventional MRI. Although conventional MRI including CE-T1 weighted image has been widely used in pre- and post-operative assessment of brain tumor, several researchers reported its limited capability of glioma-grading.<sup>2,3</sup> Our result may suggest that these two imaging sequences can give us additional information of brain tumor even without contrast materials.

Interestingly, metabolite ratios to creatine showed either better correlation with APT value or diagnostic capability of glioma grading than the concentration. The reason is hard to explain. Previous study suggested that measuring concentration of metabolites in brain tumor might be difficult, especially in high-grade glioma.<sup>34</sup> Metabolite ratios are frequently used in MRS studies and assumed as an internal standard, can give us

1 more accurate information in grading glioma than absolute concentration.<sup>35</sup> Our results  
2 may be in line with this.

3 Our study shows several limitations. First, despite several researches including  
4 current study, the origin of APT signal still remains unclear. Many researchers have  
5 demonstrated some biological signature such as cytosolic protein including folding  
6 status or amount of specific protein contributes APT signal.<sup>36,37</sup> Furthermore, there are  
7 some discussions about the confounding effects of asymmetry of the solid-phase MT  
8 effect and possible intra- and intermolecular nuclear Overhauser effects (NOE) of  
9 aliphatic protons and T1 value of the tissue to APT-weighted image.<sup>38</sup> Some authors  
10 implied or demonstrated that the background MT asymmetry or NOE effects are  
11 negligible on 3T,<sup>10</sup> while others argue that MT asymmetry is more significant than APT  
12 effect even on 3T.<sup>38</sup> According to the recent researches with ultra-high field MRI, NOE  
13 imaging has potential to delineate portion with high cellularity, or BBB disruption in  
14 glioma without contrast agents.<sup>39,40</sup> MT contrast in the brain tumor has been reported to  
15 be decreased compared with white matter, and correlate with nuclear density.<sup>41</sup> To  
16 investigate the association among NOE, MT asymmetry and metabolites in brain tumors,  
17 further studies at ultra-high field MRI may be needed. Environmental factors such as  
18 pH and temperature also have great effects on CEST image. pH imaging, which is a

1 cutting-edge application of CEST, and may become a potential marker of hypoxia.<sup>42</sup>

2 Recent study showed the promising result of amine-proton based CEST images, which

3 is focusing on 3 ppm, in detecting intratumoral pH changes.<sup>43</sup> However, this effect is

4 somewhat confusing in the assessment of brain tumor with APT images; High-grade

5 tumors with high proliferation activity can show acidotic changes due to anaerobic

6 metabolism or necrosis, which causes lactate peak in MRS.<sup>44</sup> However, such acidotic

7 change decreases the rate of proton exchange, and theoretically lessen the signal of

8 tumors on APT image. Longo et al recently demonstrated this “Warburg effect” in the

9 breast cancer model mice, using two-different modalities such as positron emission

10 tomography and pH-oriented CEST image with iopamidol as an exogenous CEST

11 contrast agent.<sup>45</sup> APT image combined with MRS, especially chemical shift imaging

12 including lactate peak may also offer complementary spatial information of tumor

13 microenvironment including pH and metabolism. Recent post-processing advance, such

14 as MT and relaxation-normalized APT, may give us additional information about

15 intratumoral pH change.<sup>46</sup> Second, we did not adjust for APT imaging using controls,

16 such as contralateral normal-appearing white matter. Such adjustment might be useful

17 for minimizing the effects of native  $MTR_{\text{asym}}$  discussed above. However, several studies

18 have shown that diagnostic capability did not differ between imaging with and without

1 such adjustment.<sup>9,11</sup> In addition, some high-grade tumors may invade diffusely, leaving  
2 little normal-appearing white matter.<sup>47</sup> Third, some cases with glioblastoma showed  
3 relatively high Cramer Rao Lower Bounds (CRLB) (%SD is more than 15) in NAA  
4 value. High grade gliomas often show low NAA peak due to glial cell invasion, as a  
5 result, fitting of low amount of total NAA concentration may be difficult. Although  
6 NAA with larger CRLB in cases with glioblastoma might be unreliable and less  
7 reproducible, exclusion of cases with glioblastoma were not beneficial in this study.  
8 Strength of this study was the fact that, to clarify the correlation, volume of interest was  
9 placed at the same location as the tumor on both MRS and APT imaging. To verify these  
10 correlations, a further study with direct comparison of histology obtained from  
11 stereotactic biopsy based on combined analysis using MRS and APT imaging may be  
12 warranted.

13 In conclusion, significant correlations were observed between metabolite  
14 concentrations and ratios on MRS and APT values. MRS and APT imaging showed  
15 comparable diagnostic capability for grading brain tumors, suggesting that both MRS  
16 and APT imaging offer potential for assessing the proliferative activity of brain tumors  
17 on non-contrast MRI.

Table 1. Patient Characteristics

| Case | Age | Sex | Histology<br>Diagnosis | Histology<br>Grade | CE  | Cho  | NAA  | Cr   | APT <sub>mean</sub><br>(%) | APT <sub>90</sub><br>(%) | APT<br>std | APT<br>skewness | APT<br>kurtosis |
|------|-----|-----|------------------------|--------------------|-----|------|------|------|----------------------------|--------------------------|------------|-----------------|-----------------|
| 1    | 57  | M   | DA                     | 2                  | +ve | 1.86 | 4.65 | 5.92 | 2.03                       | 8.18                     | 0.11       | -0.24           | 3.28            |
| 2    | 70  | F   | AA                     | 3                  | +ve | 3.60 | 3.91 | 5.23 | 4.31                       | 7.16                     | 0.05       | 0.56            | 3.18            |
| 3    | 35  | M   | Oligo                  | 2                  | -ve | 1.89 | 3.64 | 4.69 | 0.05                       | 2.74                     | 0.05       | 0.19            | 3.03            |
| 4    | 49  | M   | AO                     | 3                  | -ve | 1.84 | 2.60 | 3.68 | 0.99                       | 5.61                     | 0.11       | -0.67           | 3.75            |
| 5    | 72  | M   | GBM                    | 4                  | +ve | 8.66 | 3.55 | 4.39 | 3.28                       | 7.26                     | 0.09       | -0.22           | 3.73            |
| 6    | 71  | M   | DA                     | 2                  | -ve | 0.92 | 2.99 | 4.79 | -1.36                      | 0.41                     | 0.04       | 0.09            | 2.46            |
| 7    | 44  | F   | Oligo                  | 2                  | +ve | 1.31 | 2.21 | 3.54 | 2.46                       | 6.20                     | 0.06       | 0.13            | 2.49            |
| 8    | 27  | M   | GBM                    | 4                  | +ve | 0.79 | 0.56 | 0.70 | 3.55                       | 6.61                     | 0.07       | -0.14           | 2.41            |

|    |    |   |                |   |     |       |      |       |       |       |      |       |      |
|----|----|---|----------------|---|-----|-------|------|-------|-------|-------|------|-------|------|
| 9  | 27 | M | OA             | 2 | +ve | 1.28  | 0.72 | 2.63  | 3.47  | 7.61  | 0.05 | 0.38  | 2.80 |
| 10 | 62 | F | GBM            | 4 | +ve | 0.87  | 0.00 | 0.67  | 3.51  | 6.69  | 0.04 | 0.29  | 3.28 |
| 11 | 67 | M | DA             | 2 | -ve | 1.81  | 4.13 | 5.20  | 0.23  | 1.72  | 0.04 | 0.08  | 2.51 |
| 12 | 64 | F | GBM            | 4 | +ve | 12.83 | 0.20 | 6.23  | 2.72  | 7.75  | 0.07 | 0.42  | 5.09 |
| 13 | 80 | M | DA             | 2 | +ve | 1.12  | 3.36 | 4.98  | 0.60  | 5.43  | 0.13 | -0.81 | 3.00 |
| 14 | 11 | F | AA             | 3 | +ve | 15.10 | 4.02 | 10.62 | 5.46  | 7.95  | 0.06 | -0.22 | 2.66 |
| 15 | 24 | M | Oligo          | 2 | +ve | 2.45  | 8.95 | 8.99  | -0.31 | 5.13  | 0.08 | 0.04  | 3.84 |
| 16 | 38 | M | GBM<br>(Rec)   | 4 | +ve | 6.00  | 0.17 | 6.25  | 4.91  | 10.58 | 0.14 | 0.52  | 2.23 |
| 17 | 44 | M | Oligo<br>(Rec) | 2 | +ve | 2.48  | 0.00 | 1.25  | 1.99  | 8.76  | 0.20 | -1.22 | 4.61 |

|    |    |   |       |   |     |      |      |      |       |       |      |       |      |
|----|----|---|-------|---|-----|------|------|------|-------|-------|------|-------|------|
| 18 | 44 | F | GBM   | 4 | +ve | 3.29 | 0.00 | 3.40 | 2.94  | 6.90  | 0.13 | -0.96 | 3.26 |
| 19 | 34 | M | GBM   | 4 | +ve | 1.79 | 1.67 | 2.80 | 0.87  | 7.86  | 0.10 | 0.28  | 3.16 |
| 20 | 85 | F | GBM   | 4 | +ve | 2.85 | 3.66 | 4.48 | -1.75 | 10.65 | 0.24 | -1.27 | 5.10 |
| 21 | 46 | F | Oligo | 2 | -ve | 2.28 | 8.02 | 6.89 | -2.52 | 3.85  | 0.08 | -0.43 | 4.35 |

std, standard deviation; DA, Diffuse Astrocytoma; AA, Anaplastic Astrocytoma; OA, Oligoastrocytoma; AO, Anaplastic oligoastrocytoma; GBM, Glioblastoma; Oligo, Oligodendroglioma; Rec, recurrence; CE +ve represents positive contrast enhancement, and CE -ve represents negative contrast enhancement; LG, Low-Grade diagnosed by neuroradiologist; HG, High-Grade diagnosed by neuroradiologist.

Table 2. The correlation among parameters obtained by MRS and APT histogram analysis

|                     | Cho                       | NAA               | Cho/Cr              | NAA/Cr              |
|---------------------|---------------------------|-------------------|---------------------|---------------------|
| $APT_{\text{mean}}$ | 0.23 (p=0.32)<br>(p=0.32) | -0.43<br>(p=0.05) | 0.65*<br>(p=0.0015) | -0.52*<br>(p=0.016) |
| $APT_{90}$          | 0.49*<br>(p=0.025)        | -0.31<br>(p=0.17) | 0.59*<br>(p=0.005)  | -0.37<br>(p=0.098)  |

|                         | Cho               | NAA               | Cho/Cr           | NAA/Cr            |
|-------------------------|-------------------|-------------------|------------------|-------------------|
| $APT_{\text{std}}$      | 0.33<br>(p=0.15)  | -0.19<br>(p=0.42) | 0.13<br>(p=0.58) | 0.06<br>(p=0.78)  |
| $APT_{\text{skewness}}$ | -0.05<br>(p=0.84) | -0.14<br>(p=0.54) | 0.1<br>(p=0.67)  | -0.24<br>(p=0.29) |
| $APT_{\text{kurtosis}}$ | 0.39<br>(p=0.08)  | 0.04<br>(p=0.63)  | 0.23<br>(p=0.32) | 0.17<br>(p=0.47)  |

std, standard deviation

\*  $p$  value < 0.05

Table 3. AUC values in ROC analysis for grading glioma with contrast enhancement on T1-weighted imaging, MRS, and APT imaging.

| Parameters           | Area Under the Curve | 95% Confidence Interval |
|----------------------|----------------------|-------------------------|
| Contrast Enhancement | 0.65                 | 0.47 to 0.84            |
| APT <sub>mean</sub>  | 0.82                 | 0.62 to 1.00            |
| APT <sub>90</sub>    | 0.77                 | 0.54 to 1.00            |
| Cho                  | 0.72                 | 0.47 to 0.97            |
| Cho/Cr               | 0.90                 | 0.73 to 1.00            |

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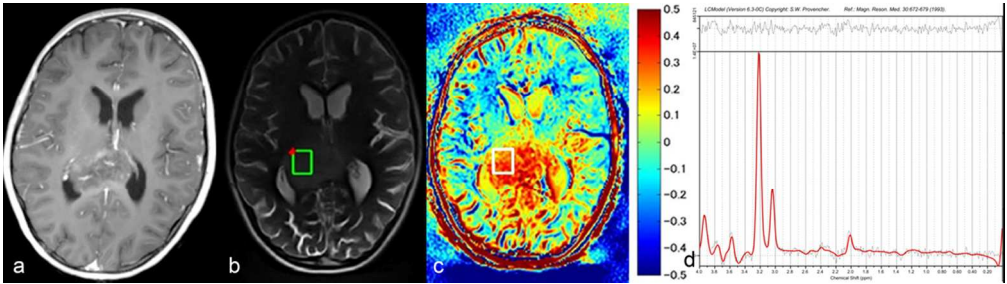
1992;34:331-333.

## Figure Legends

**Fig. 1** An 11-year-old boy diagnosed as anaplastic astrocytoma (Patient #14). The tumor at the corpus callosum shows tiny enhancement on CE T1-weighted image (a). VOI for MRS was placed on the area showing the solid portion of tumor on T2-weighted image (source image of APT imaging) (b). The VOI was automatically transferred to the APT image by in-house MATLAB script (c). On APT image, the tumor shows increased signal in the corpus callosum. (d) LCModel analysis shows elevation of Cho and decreased NAA. These findings are compatible with high-grade brain tumor.

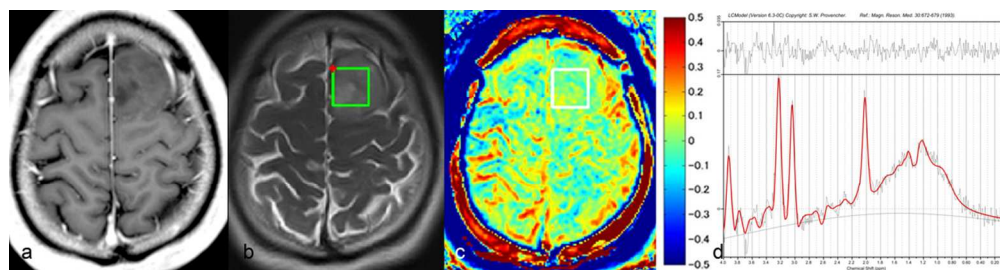
**Fig. 2** A 35-year-old male diagnosed as oligodendroglioma (Patients #3). The tumor shows no enhancement on CE T1-weighted image (a). VOI for MRS was placed on the area showing the solid portion of tumor on T2-weighted image (source image of APT imaging) (b). On APT image, the tumor in the left frontal lobe shows similar signal intensity to that of the contralateral normal white matter (c). LCModel analysis shows moderate level of Cho and NAA (d). These findings are compatible with low-grade brain tumor.

**Fig. 3** Receiver-operating-characteristics curve analysis for grading brain tumor with APT imaging, MRS and conventional MR imaging. ROC curves illustrated the performance of contrast enhancement, Cho, Cho/Cr, APT<sub>mean</sub> and APT<sub>90</sub>. APT<sub>mean</sub> cutoff of 2.72 offered the best combination of sensitivity (72.7%) and specificity (90%) in the characterization of high-grade gliomas, while the APT<sub>90</sub> cut-off of 6.61 demonstrated the optimal combination of sensitivity (90.9%) and specificity (70%). Cho/Cr threshold value of 0.50 generated the best combination of sensitivity (100%) and specificity (93.8%) in the discrimination of high- and low-grade tumors. All the imaging parameters above except Cho demonstrated higher AUC values than that of contrast enhancement (AUC was 0.65).



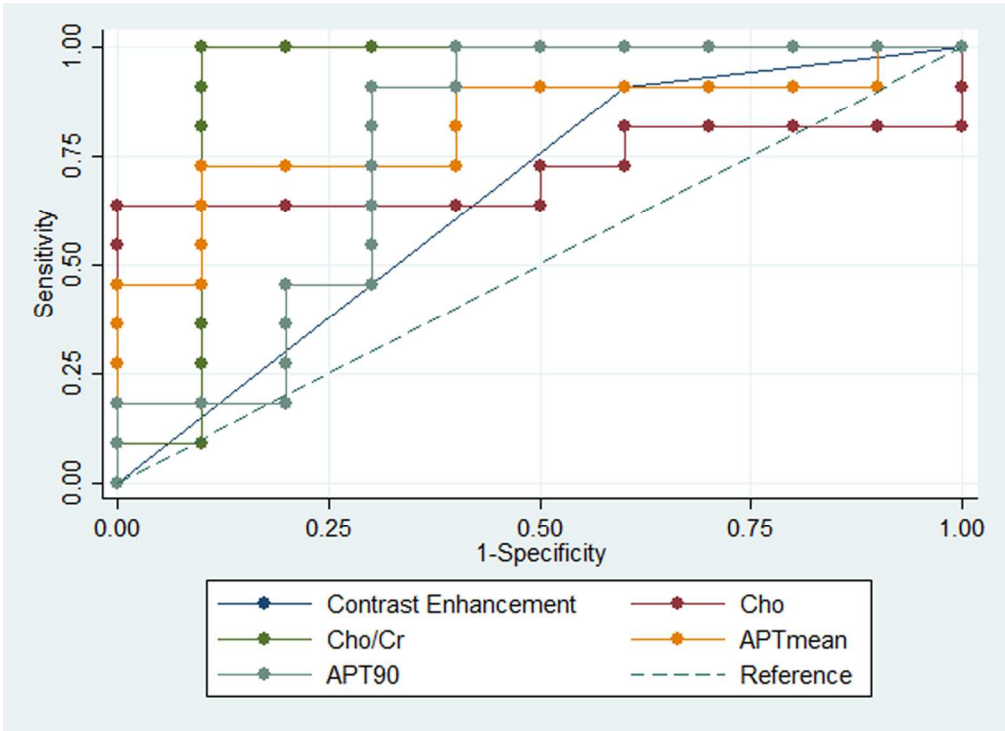
**Fig. 1.** An 11-year-old boy diagnosed as anaplastic astrocytoma (Patient #14). The tumor at the corpus callosum shows tiny enhancement on CE T1-weighted image (a). VOI for MRS was placed on the area showing the solid portion of tumor on T2-weighted image (source image of APT imaging) (b). The VOI was automatically transferred to the APT image by in-house MATLAB script (c). On APT image, the tumor shows increased signal in the corpus callosum. (d) LCMoDeR analysis shows elevation of Cho and decreased NAA. These findings are compatible with high-grade brain tumor.

108x30mm (300 x 300 DPI)



**Fig. 2.** A 35-year-old male diagnosed as oligodendroglioma (Patients #3). The tumor shows no enhancement on CE T1-weighted image (a). VOI for MRS was placed on the area showing the solid portion of tumor on T2-weighted image (source image of APT imaging) (b). On APT image, the tumor in the left frontal lobe shows similar signal intensity to that of the contralateral normal white matter (c). LCMoDeL analysis shows moderate level of Cho and NAA (d). These findings are compatible with low-grade brain tumor.

108x28mm (300 x 300 DPI)



**Fig. 3.** Receiver-operating-characteristics curve analysis for grading brain tumor with APT imaging, MRS and conventional MR imaging. ROC curves illustrated the performance of contrast enhancement, Cho, Cho/Cr, APT<sub>mean</sub> and APT<sub>90</sub>. APT<sub>mean</sub> cutoff of 2.72 offered the best combination of sensitivity (72.7%) and specificity (90%) in the characterization of high-grade gliomas, while the APT<sub>90</sub> cut-off of 6.61 demonstrated the optimal combination of sensitivity (90.9%) and specificity (70%). Cho/Cr threshold value of 0.50 generated the best combination of sensitivity (100%) and specificity (93.8%) in the discrimination of high- and low-grade tumors. All the imaging parameters above except Cho demonstrated higher AUC values than that of contrast enhancement (AUC was 0.65).

108x79mm (300 x 300 DPI)